

가속기를 이용한 방사선치료 (의학물리)

가속기학교

July 2022

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1. Accelerators for Radiation Therapy
 - x-ray
 - proton beam
 - carbon ion beam
2. An Example of Radiation Therapy
 - CT simulation
 - Radiation Therapy Planning
 - Patient Localization
 - Quality Assurance
3. Introduction to Medical Physics

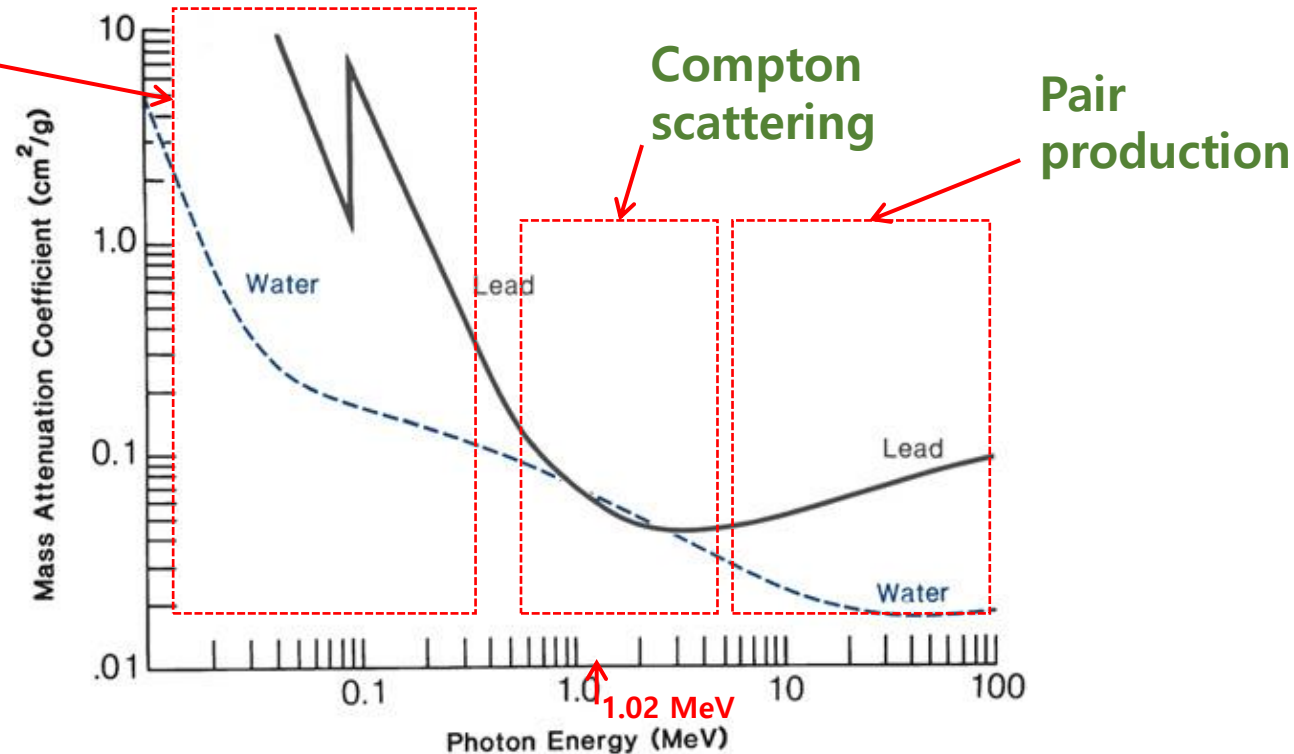
Interactions: Radiation to Matter

$$(\mu / \rho) = (\tau / \rho) + (\sigma_{coh} / \rho) + (\sigma / \rho) + (\Pi / \rho)$$

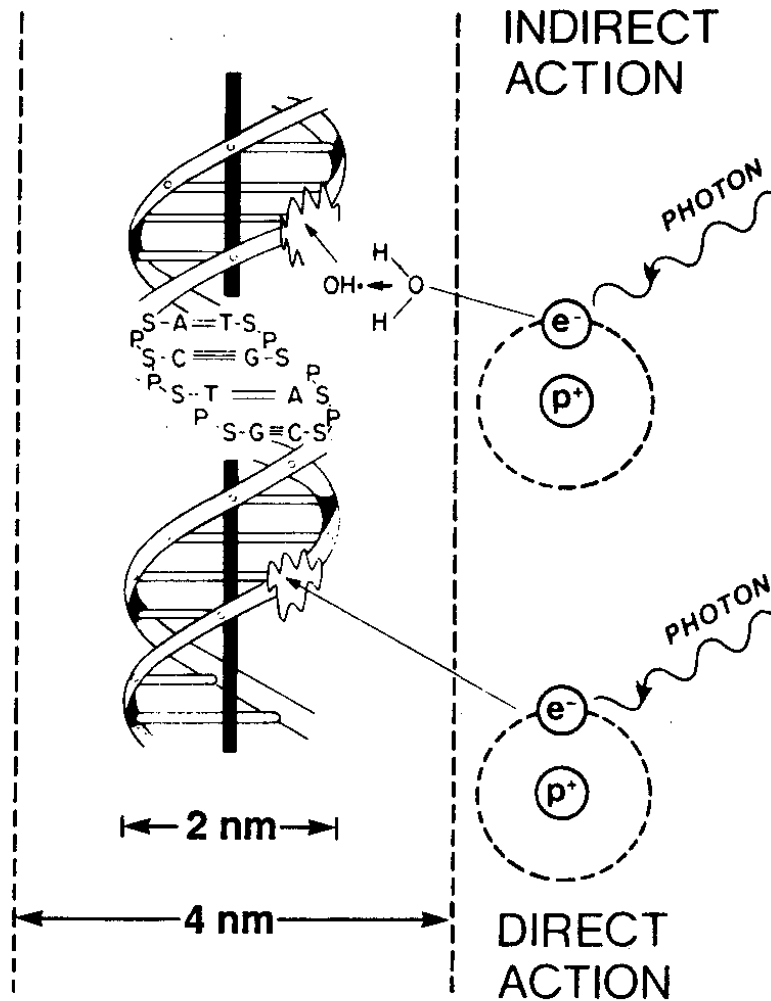
- coherent scattering: for very low photon energies (<10keV) and high Z materials

Photoelectric

$$\tau / \rho \propto Z^3 / E^3$$



종양세포에 대한 방사선 효과



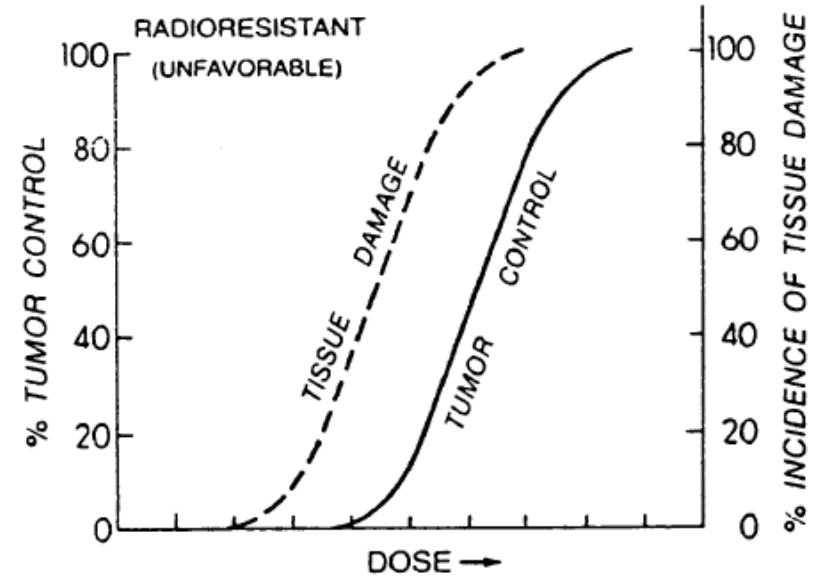
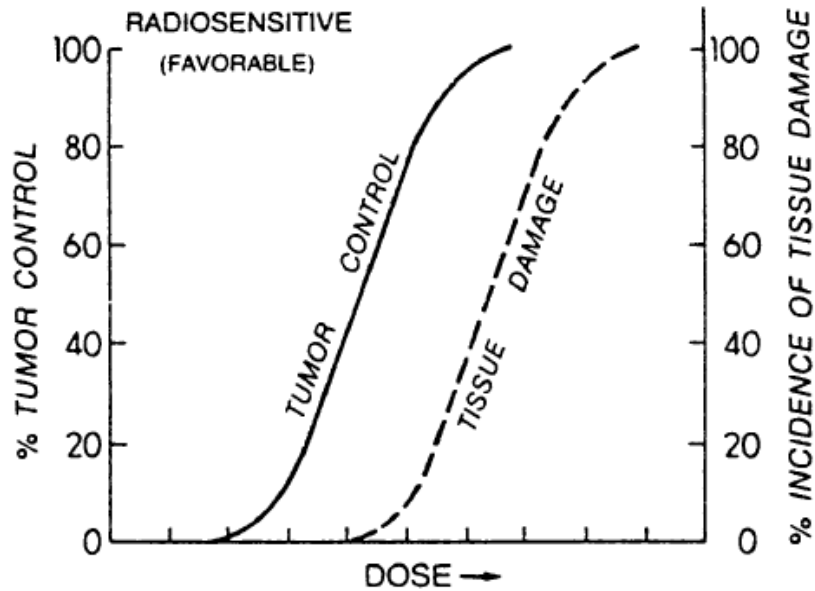
X선, γ 선 등 일반 방사선
유리기(free radical, $OH\cdot$)가 관여
산소(O_2)에 의해 DNA 손상 고착

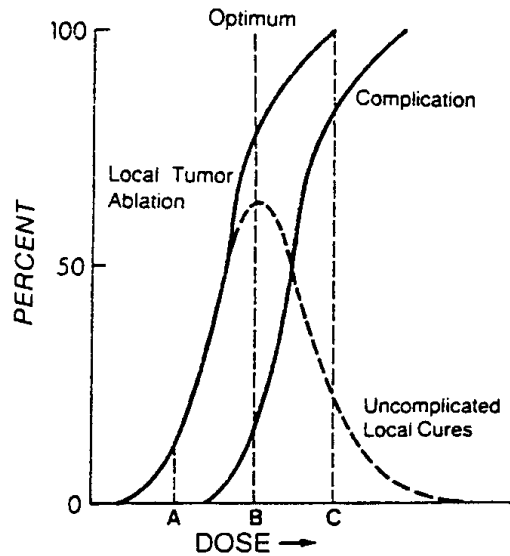
중성자선 등
산소(O_2) 필요없음

5) 방사선치료의 원리

치료비 (Therapeutic Ratio)

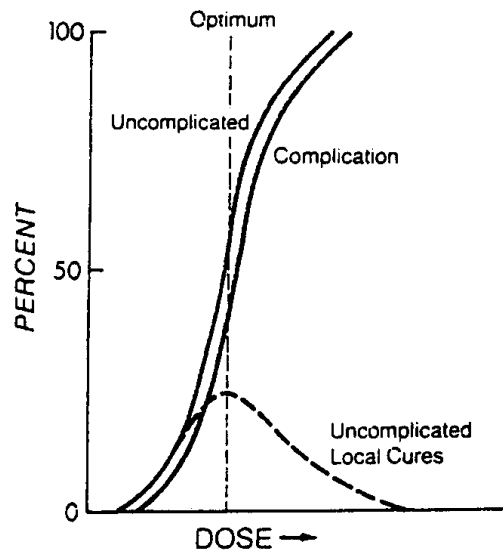
정상조직과 종양의 방사선감수성 (radiation sensitivity) 차이를 이용





정상조직과 종양간의
치료적 이득 (therapeutic gain)이 있음

	정상조직부작용	종양조절율	치료선
량			
A	(-)	↓	부적합
B	(+)	↑	적합
C	↑	최대	부적합



정상조직과 종양간의
치료적 이득 (therapeutic gain)이 거의 없
음

1. Accelerators for Radiation Therapy

Example of Medical use of Accelerators

1. Radiation Treatment

- **X-ray Radiation Therapy & Electron Therapy**

(Linear accelerator 4~25 MeV/e)

- **Proton Therapy**

(Cyclotron, Synchrotron 230 ~ 250MeV/p)

- **Carbon Therapy**

(Synchrotron 400~430MeV/u Carbon)

- **Born-Neutron Capture Therapy**

(Linear accelerator, Cyclotron 10~30 MeV/p)

2. Nuclear Medicine

- **Positron Emission Tomography**

(Cyclotron 5~ 20MeV/p)

X-rays and Electron beam

varian
A Siemens Healthineers Company

iX



Trilogy



VitalBeam



TrueBeam



Halcyon

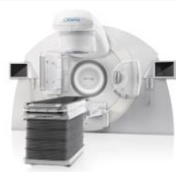


Ethos

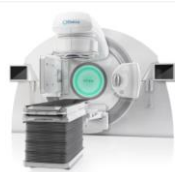


Elekta

Synergy



Infinity



VersaHD



Harmony



Unity



ACCURAY

CyberKnife



Tomotherapy Hi-Art



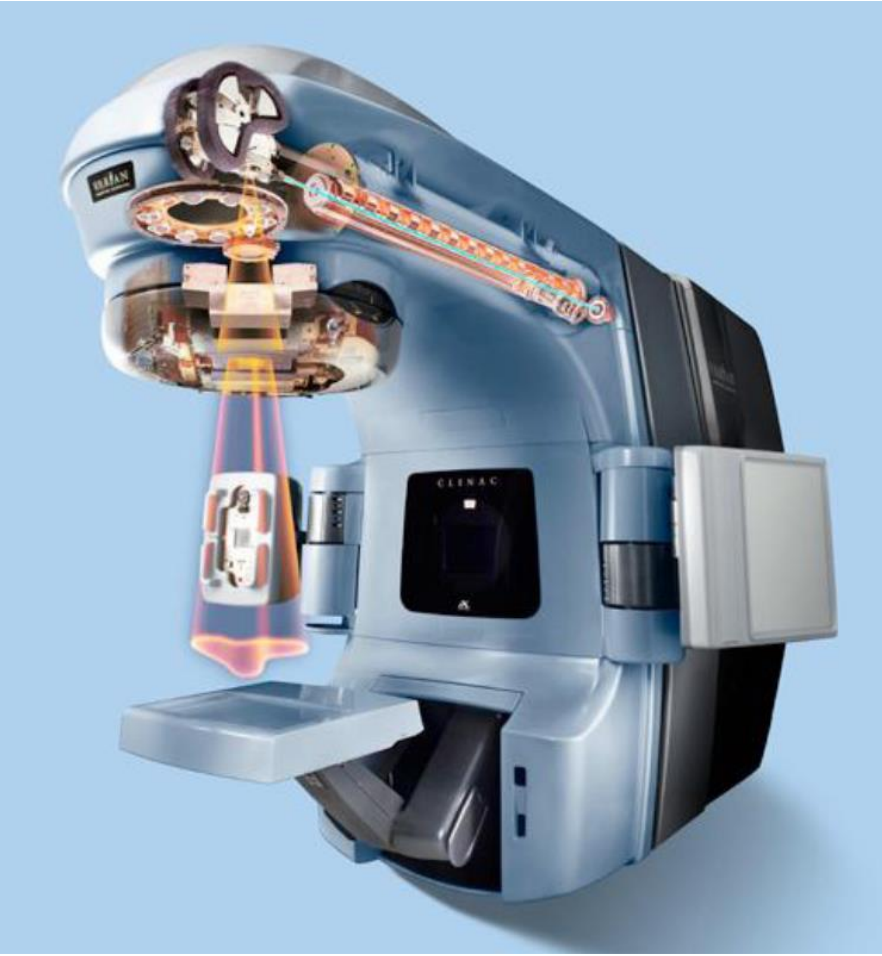
Radixact

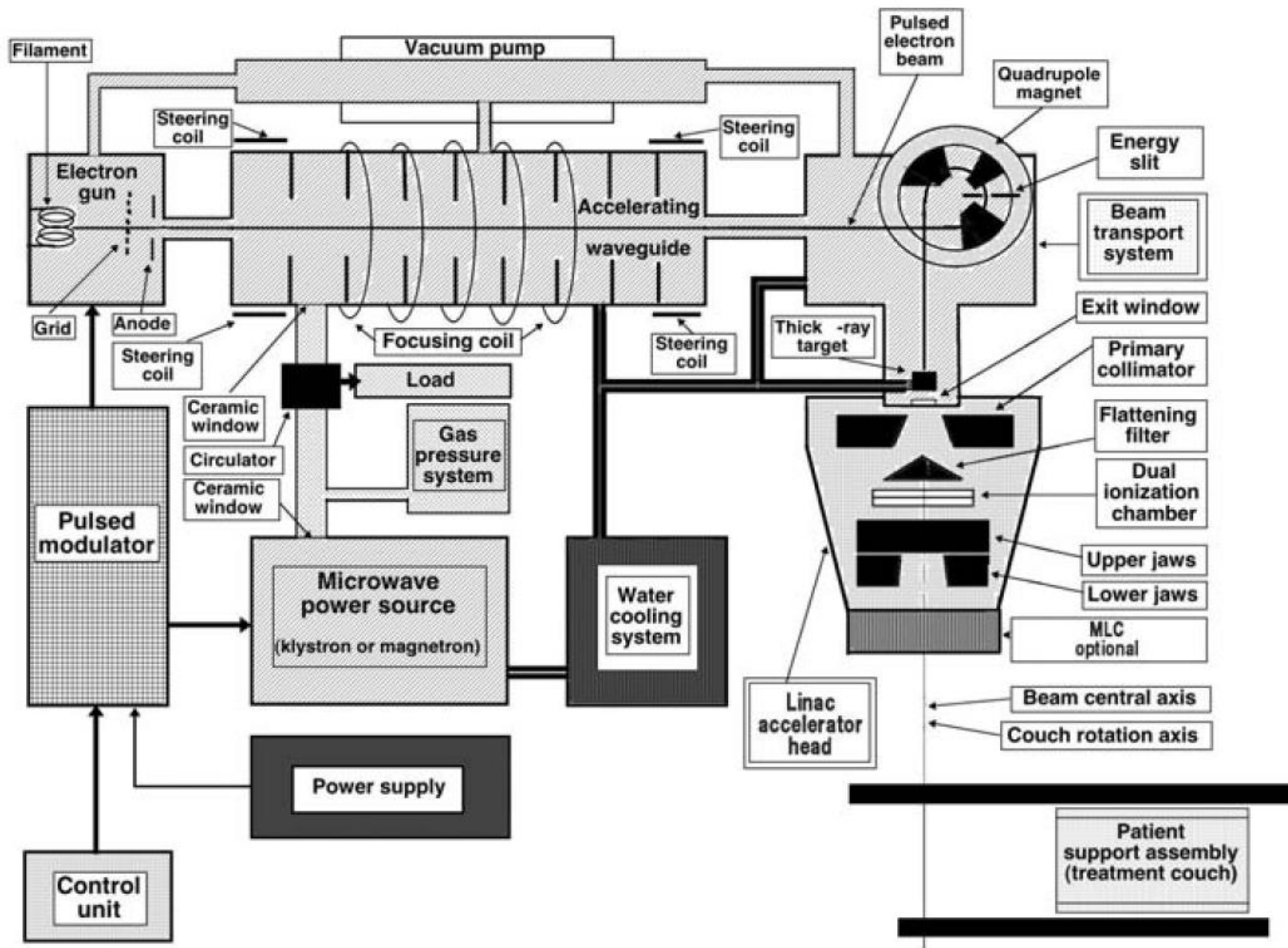


MRIdian

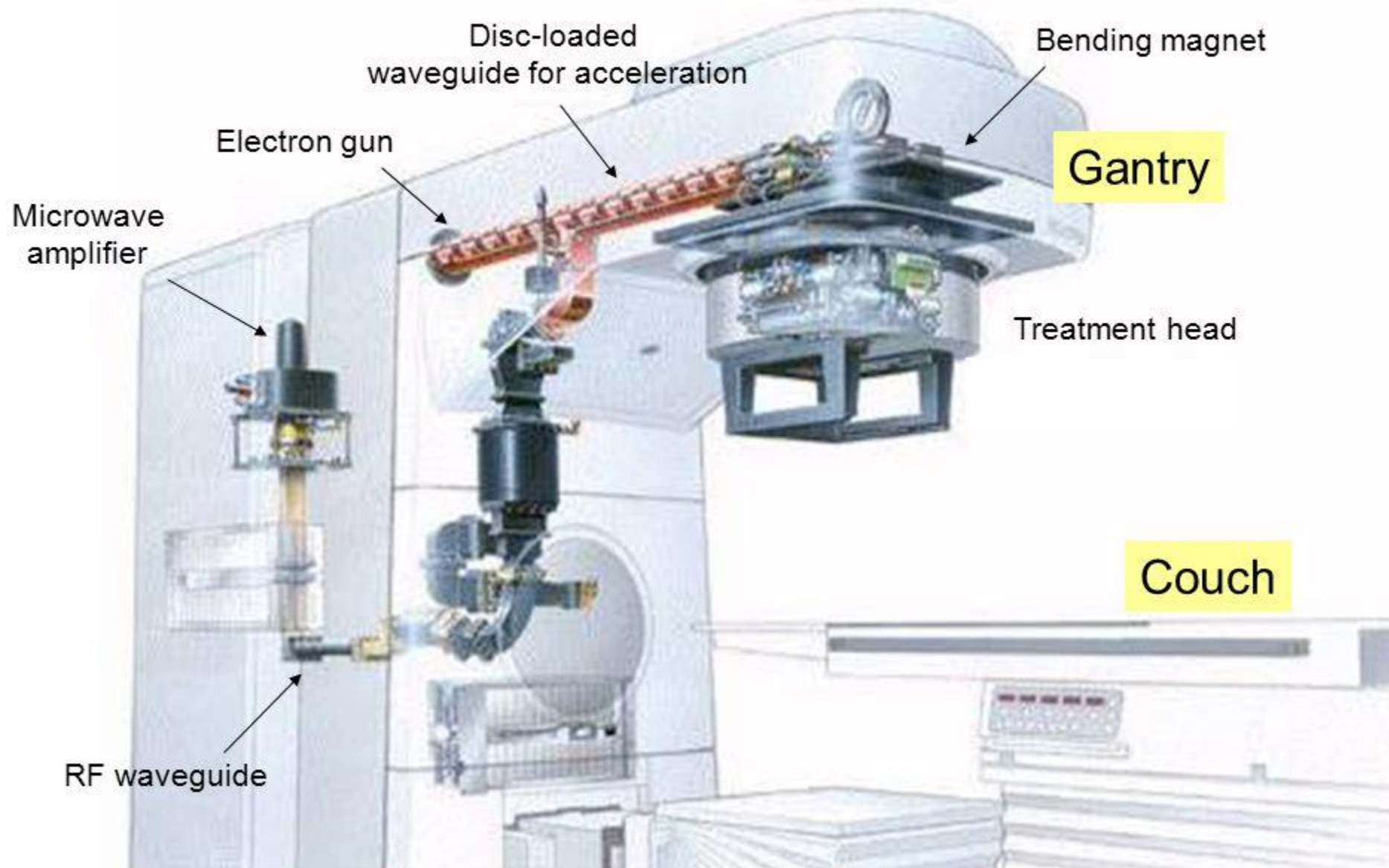


VIEWRAY
VISIBLY BETTER™





Main components of medical linac

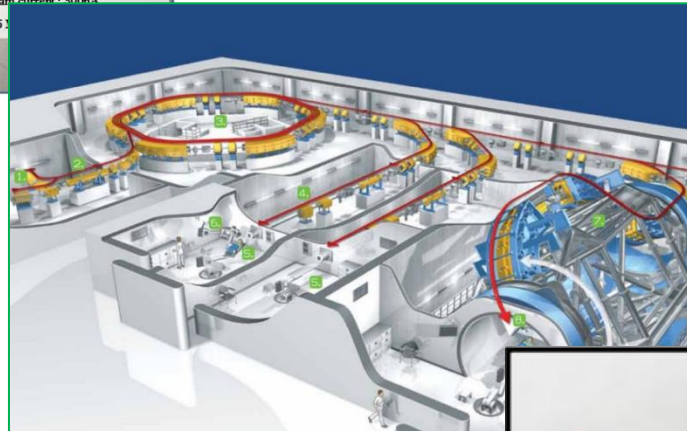


Proton Therapy

Particle Therapy Systems

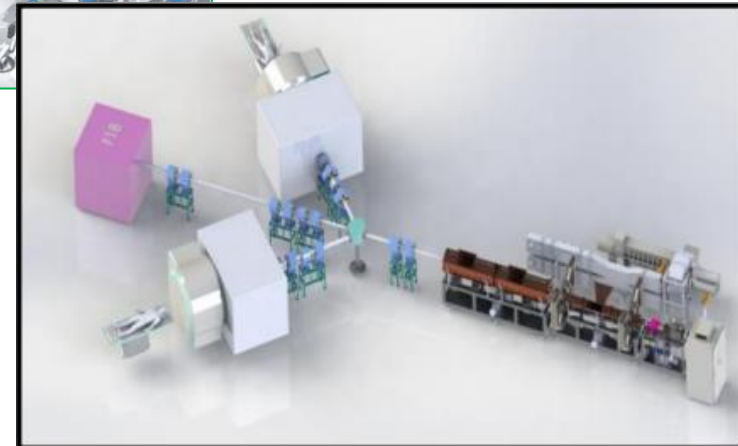


Proton Therapy

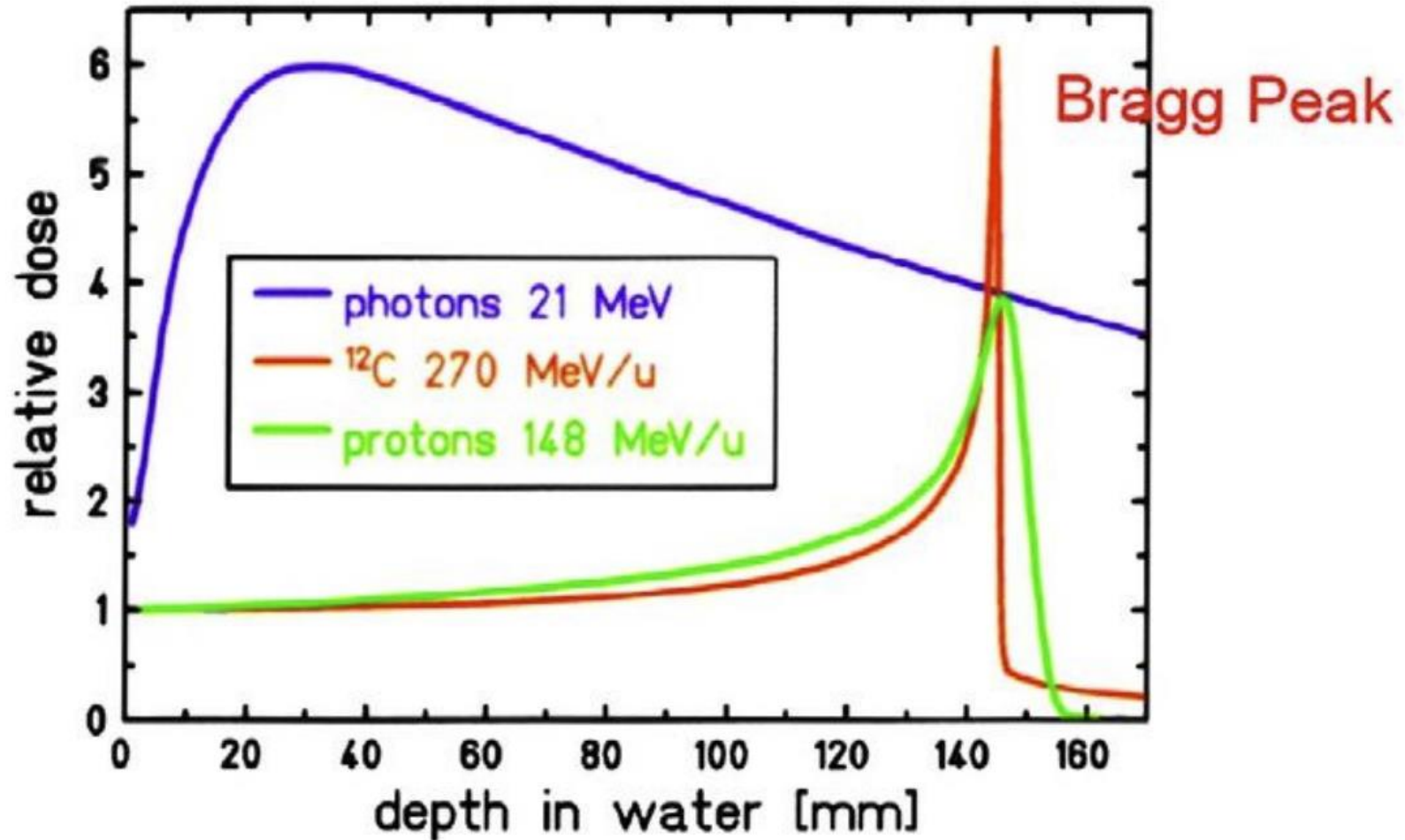


Carbon Therapy

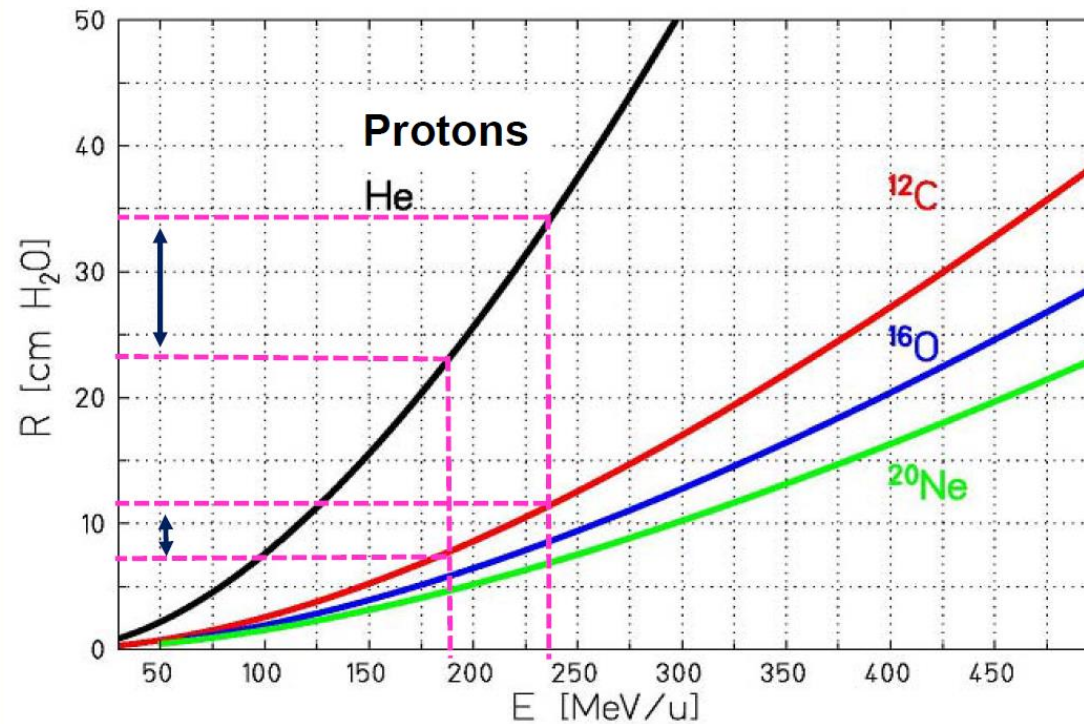
Born Neutron
Capture Therapy



Depth dose curve for radiations



Particle Range vs Energy



MASSACHUSETTS
GENERAL HOSPITAL

CANCER CENTER™

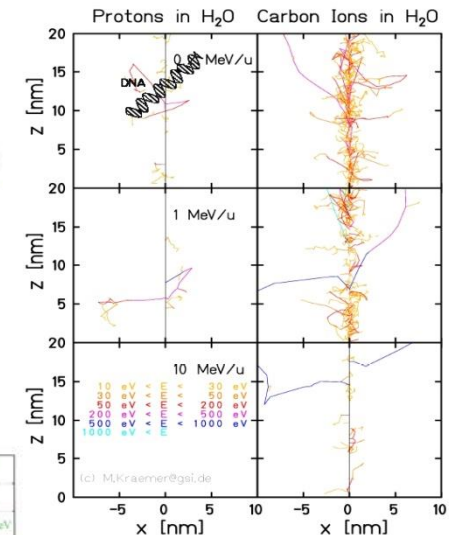
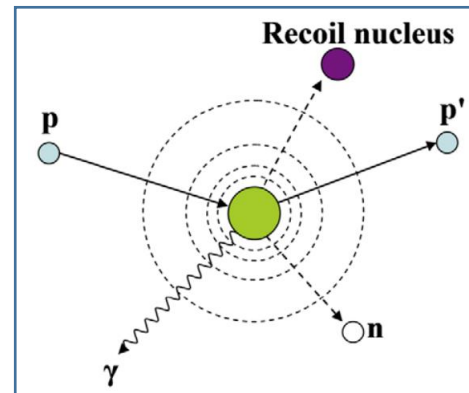
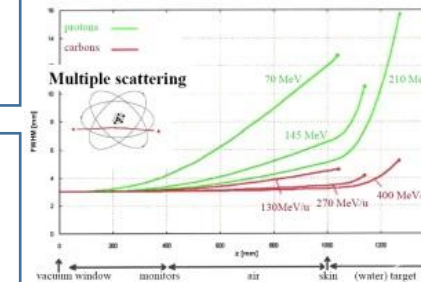
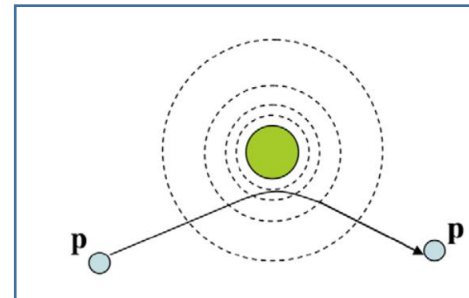
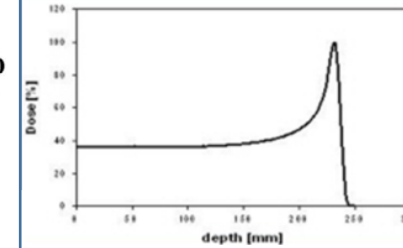
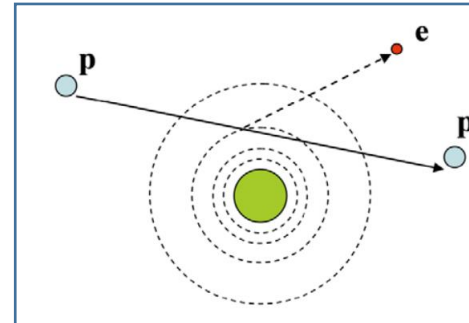


HARVARD
MEDICAL SCHOOL

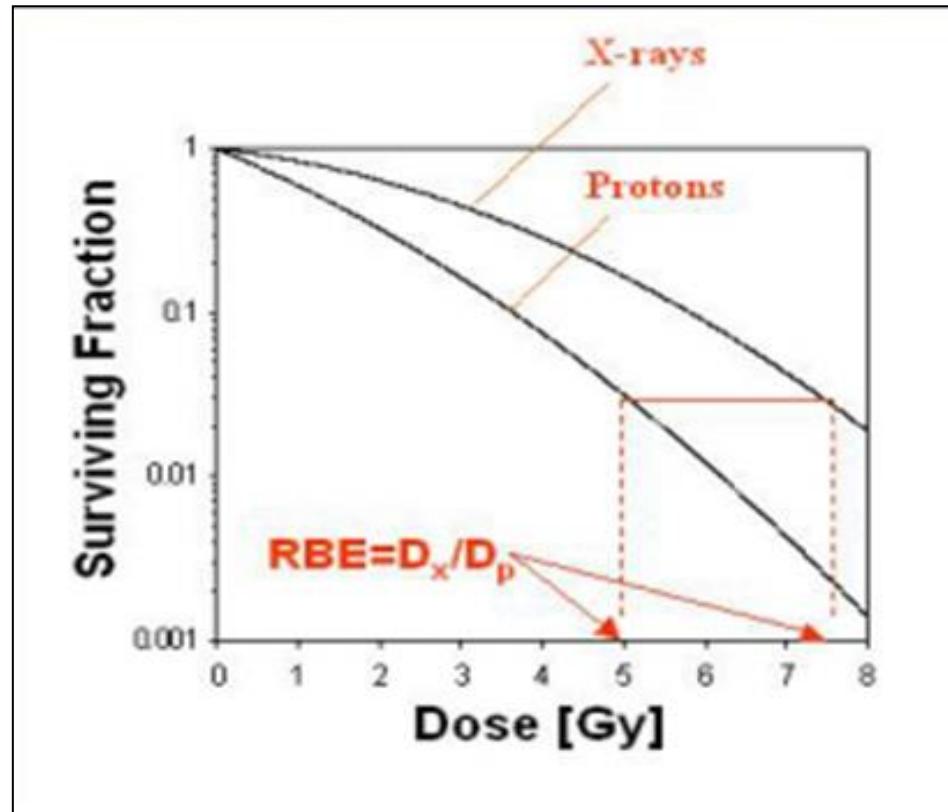
© GSI

1-2. Physics & Biology of PT

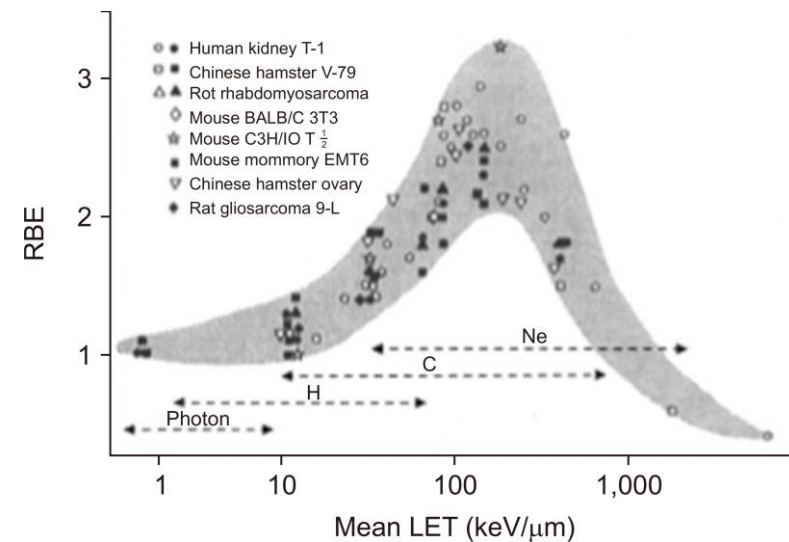
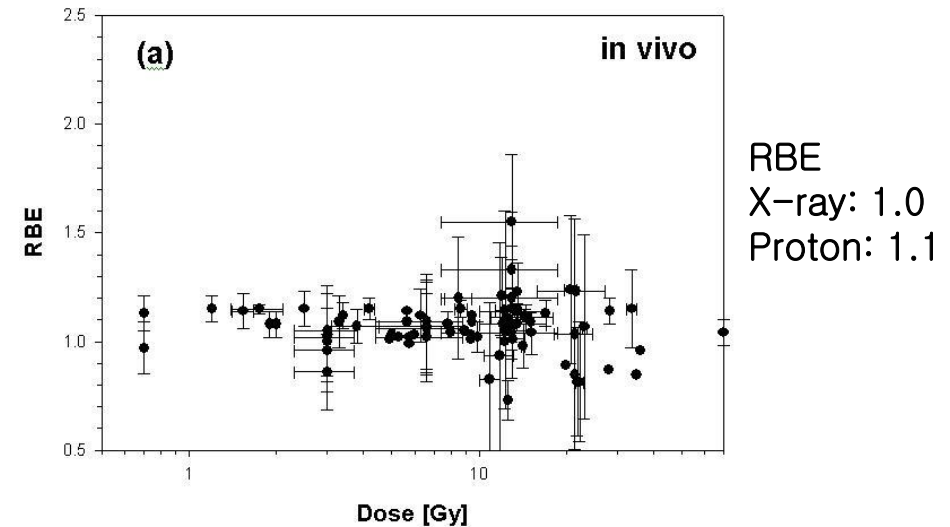
- **Electronic Process (Energy Loss)**
 - **Inelastic collisions (Ionization & Excitation)**
 - : **Bragg-Peak & Distal Penumbra**
- **Nuclear Process (Deflection, E loss)**
 - **Elastic scattering (MCS, Collision)**
 - : **Lateral Penumbra**
 - **Nuclear reactions**



Relative Biological Effectiveness (RBE)

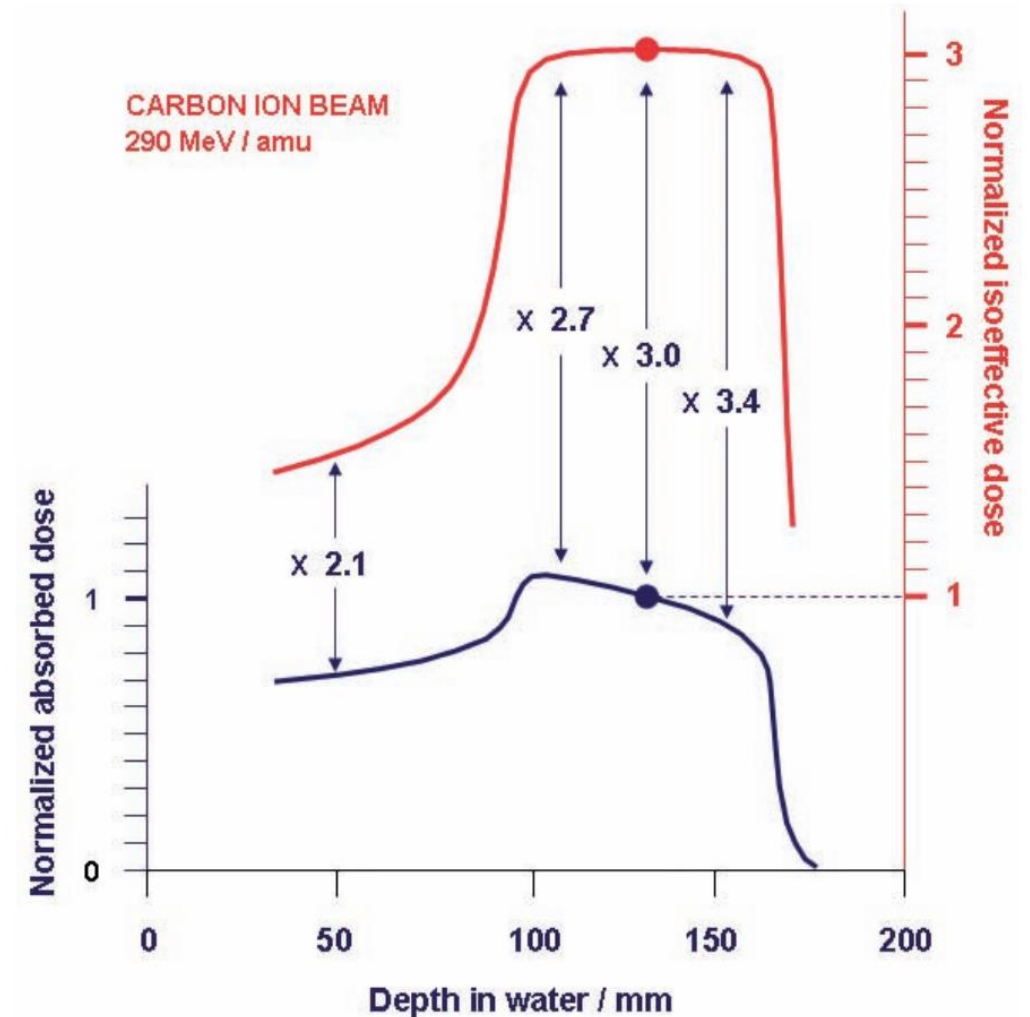
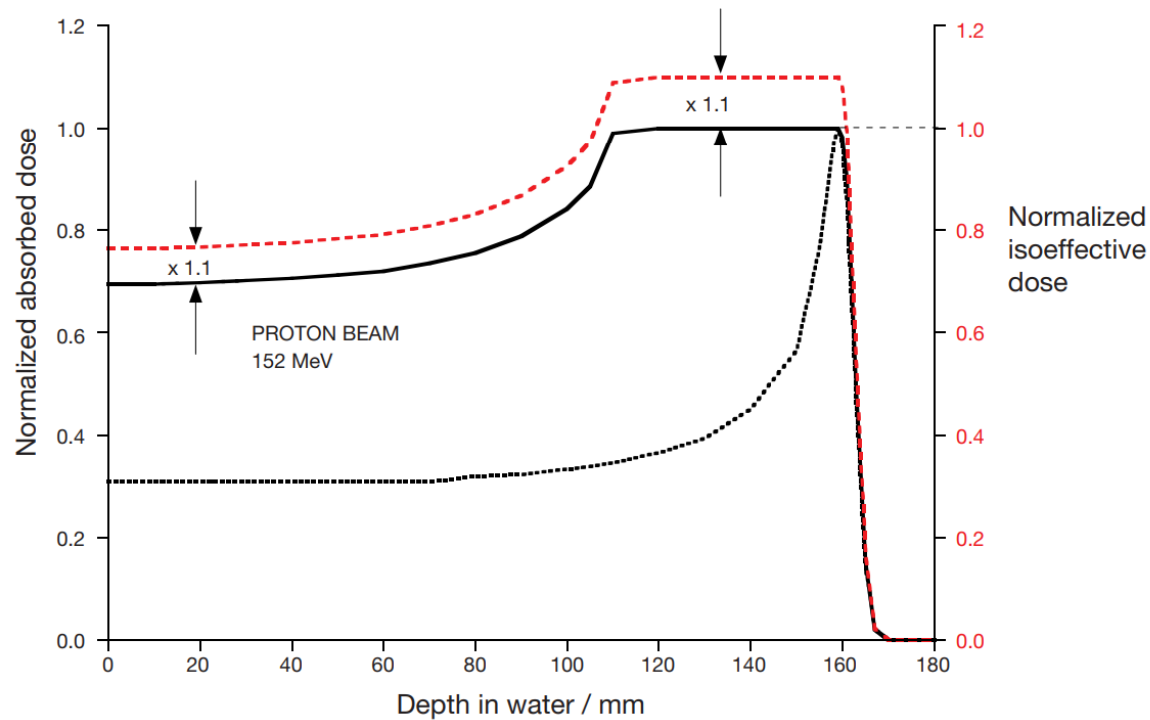


Cell survival curves to X-ray & P



RBE of proton and carbon ion beam

Proton beam

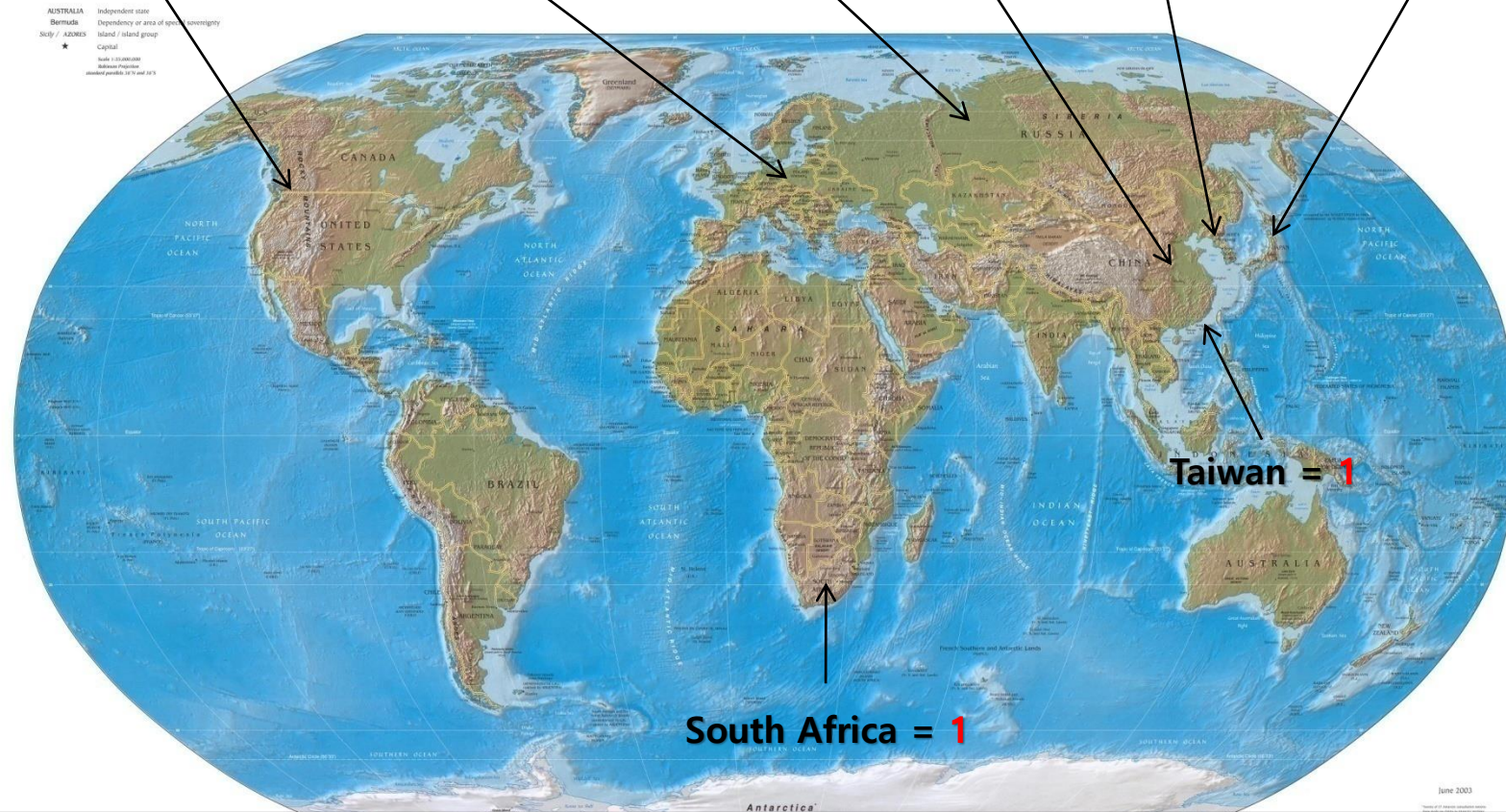


1-3. Worldwide particle therapy facilities

48 PROTON AND **9 CARBON** ION THERAPY FACILITIES IN OPERATION(2015.09)

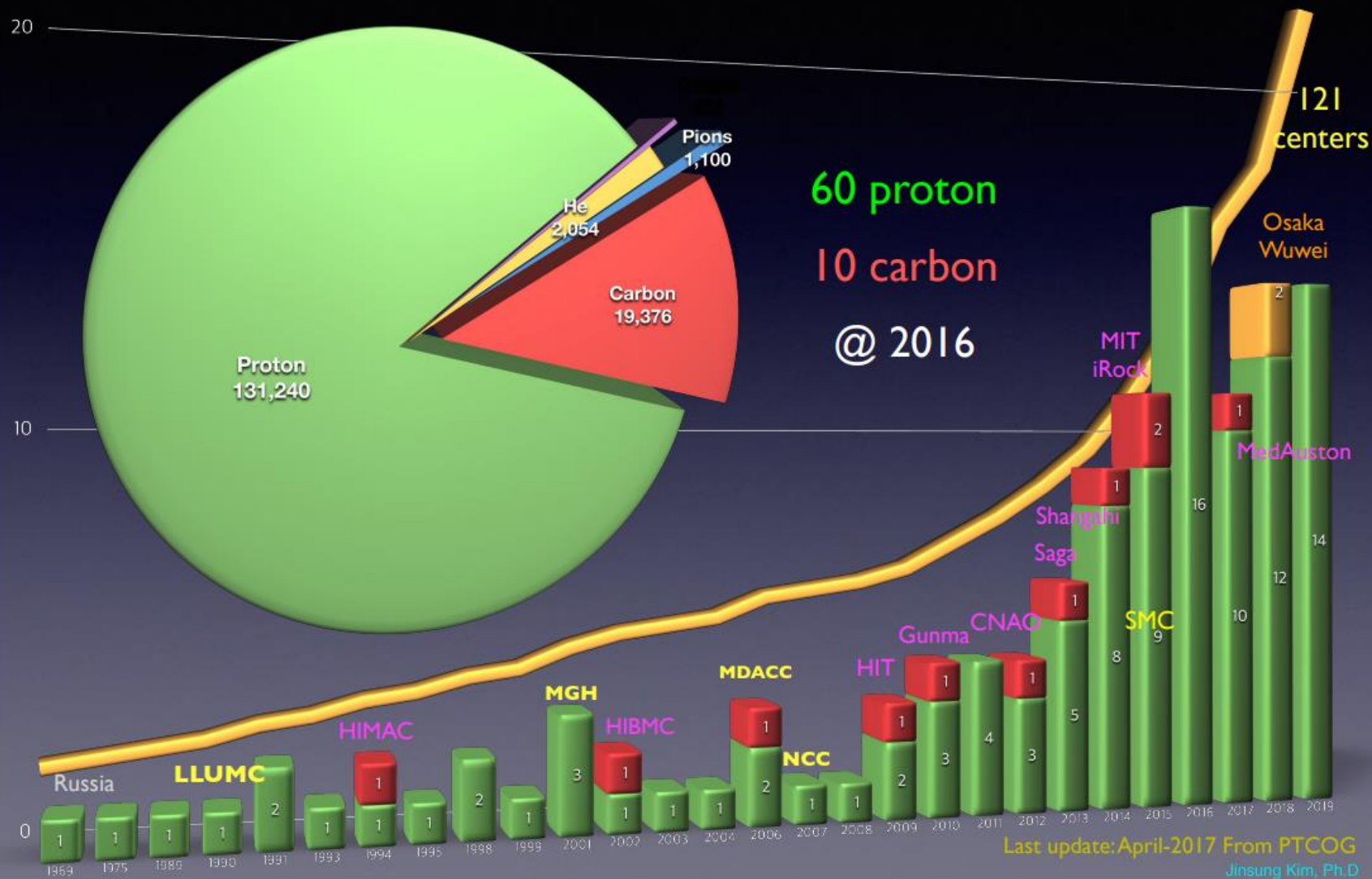
North America = **18** Europe = **15+3** Russia = **3** China = **2+2** Korea = **1** Japan = **9+4**

Physical Map of the World, June 2003



Under Construction : USA 15, Europe 8+1, Japan 3+1, China 2+1, Korea 1+1, Etc 3.
Planning stage : Worldwide 15 * Total : Proton 47 + Carbon 3

Particle Therapy Center in the world



1-4. Providers for Proton Therapy

varian
A Siemens Healthineers Company

ProBeam



ProBeam
Compact



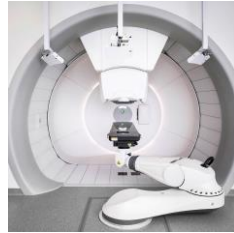
Multi Room



ProBeam360
Single Room Multi Room



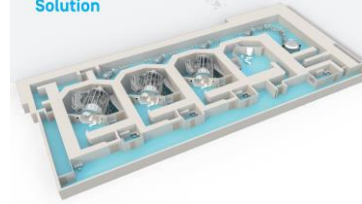
Proteus



Proteus ONE



Proteus PLUS



HITACHI
Inspire the Next

ProBEAT (proton)



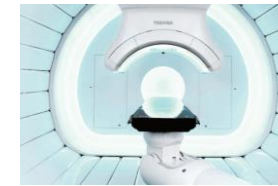
HyBEAT (carbon ion)



 **Sumitomo**
Heavy Industries, Ltd.



TOSHIBA



 **MEVION**
medical systems

S250



S250mx



 **PROTON**
proton therapy technologies



 **OPTIVUS**
PROTON THERAPY



 **ProNova** SC360



2-1. Accelerators (1)



Cyclotron



Synchrotron

2-1. Accelerators (2)

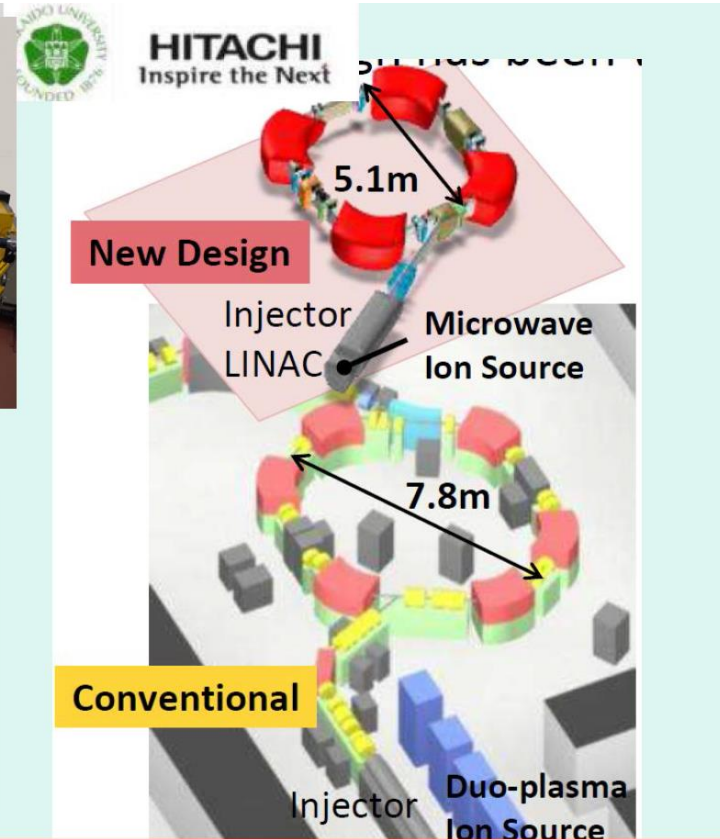
Compact synchrotron



ProTom 330 MeV

2012: Installation at:
McLaren, Flint (Mi)
MGH Boston (Ma)

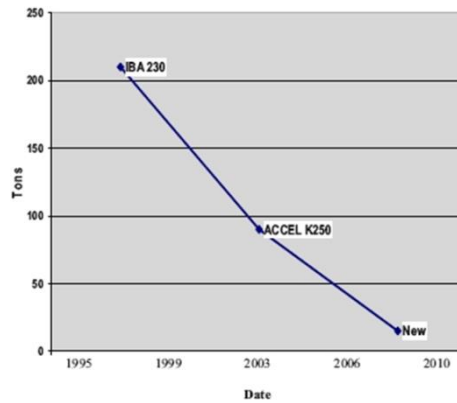
- Fully variable beam energy of 30-330 MeV $\pm$ 0.15%
- Time of acceleration up to 330 MeV - 1 sec
- Efficiency of the beam extraction $\sim$ 80%
- Total weight - 15 tons



- 220 MeV
- First facility in Hokkaido started 2013

2-1. Accelerators (3)

Synchro-Cyclotron



Cyclotron → Synchro-Cyclotron
Diameter : 4m → 1.8m
Weight : 220tons → 40tons



2~5 nA @ nozzle
10~20 nA @ Accelerator



2 Gy/min

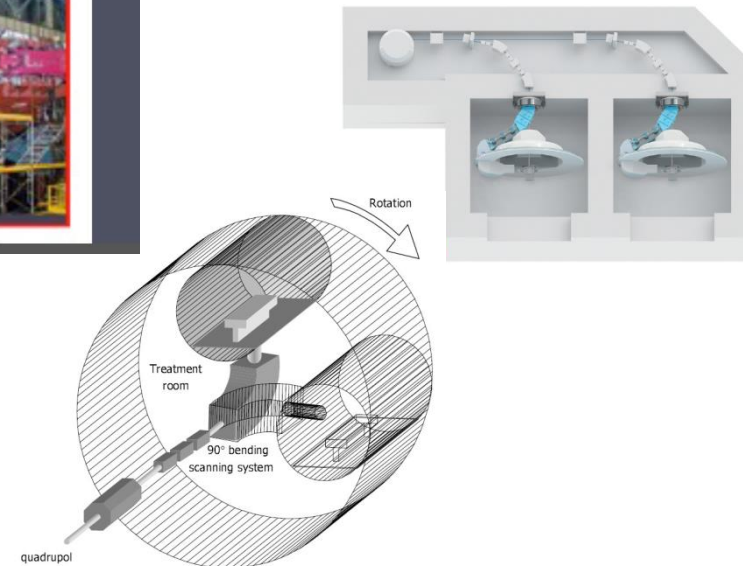
2-3. Gantry



Various Gantry Systems

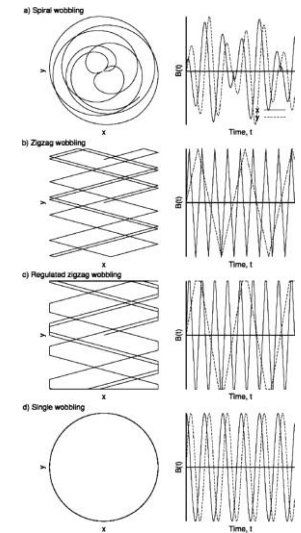
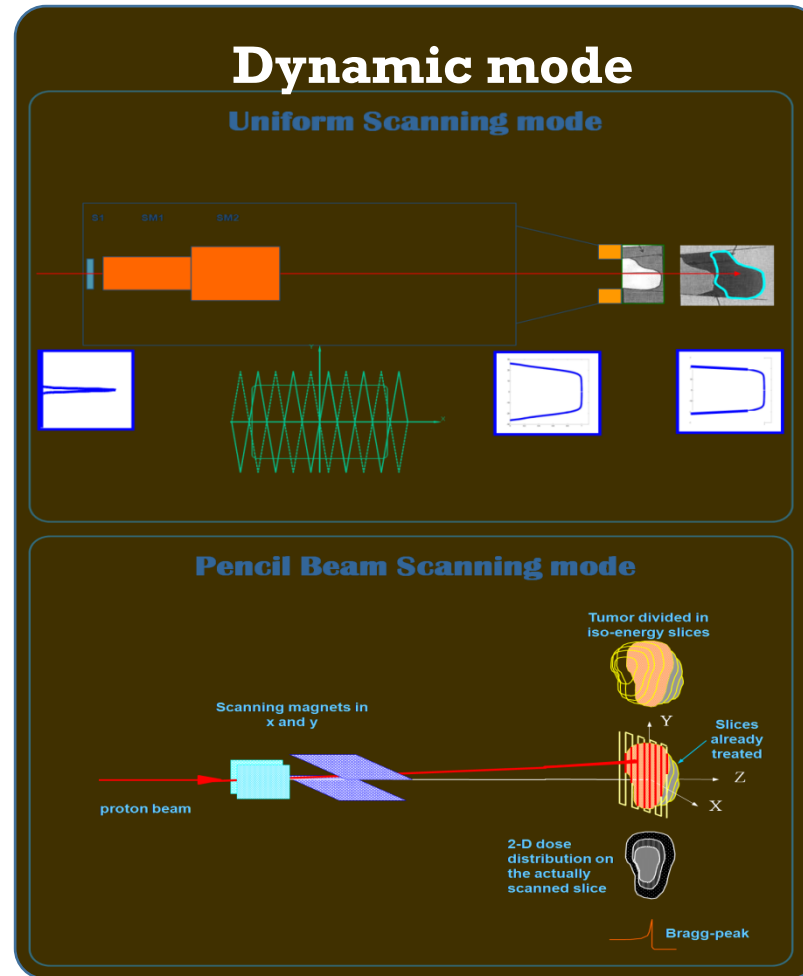
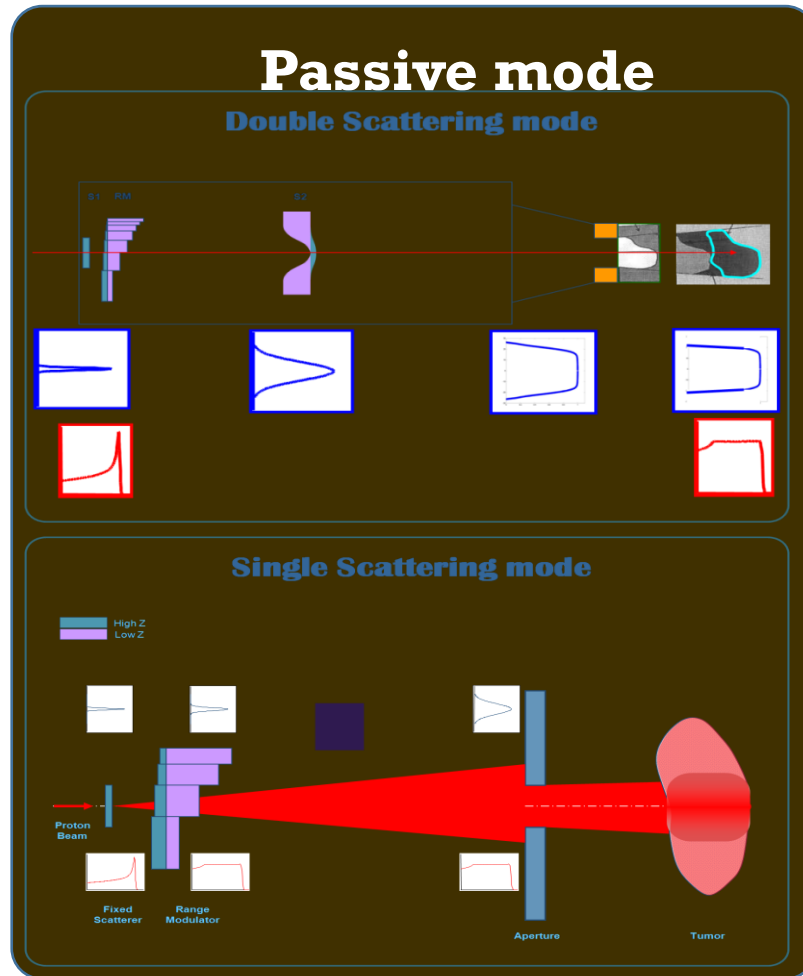


Large & Heavy →
Compact & Light Design
Still expensive..



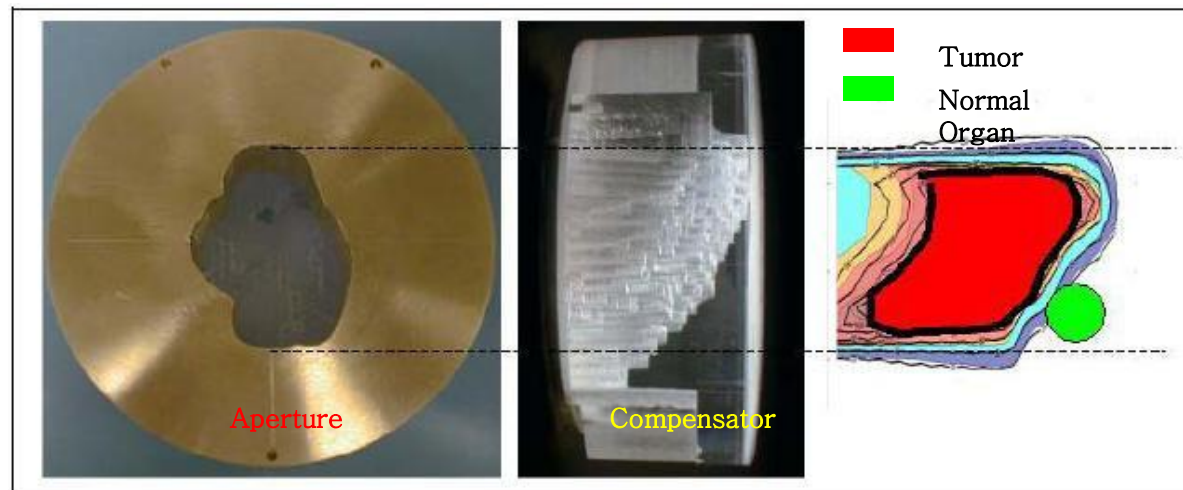
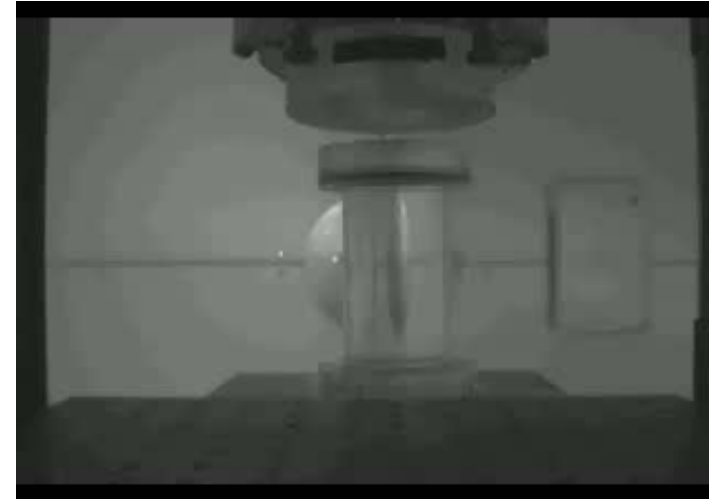
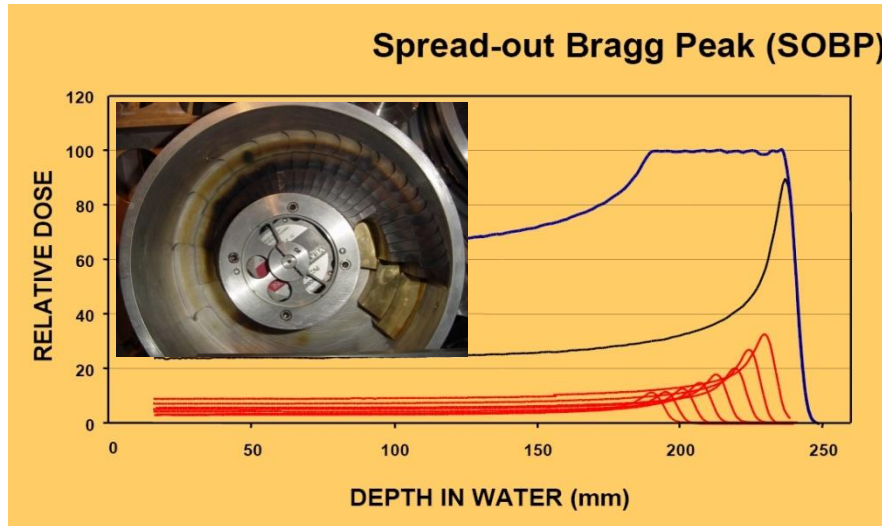
2-2. Beam Nozzle (1)

Proton Beam Delivery Modes



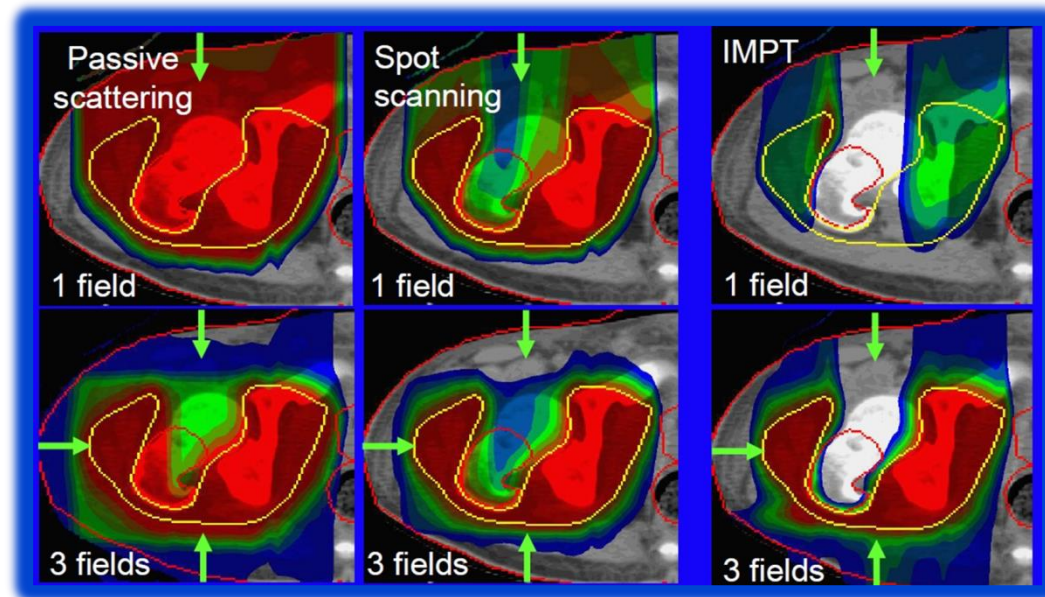
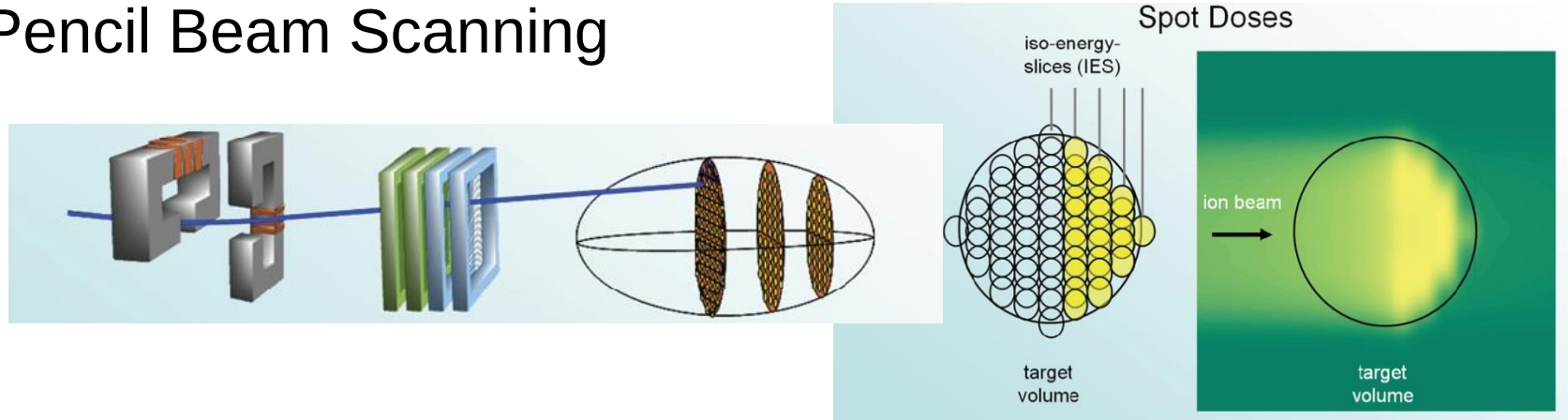
2-2. Beam Nozzle (2)

Beam Modulation (Range) & Patient dedicated Devices



2-2. Beam Nozzle (3)

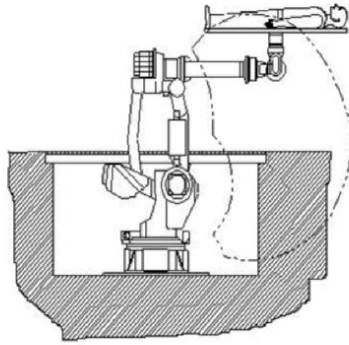
Pencil Beam Scanning



- Comparison of Dose Distribution
- Passive vs. Spot scanning vs. IMPT
 - 1field vs. 3fields

2-4. Patient Positioning System (1)

Robotic Couch



With Compliments from CPO



Forte 2008



Siemens 2005



START

CPO
1997



MPRI
2004

2-4. Patient Positioning System (2)

Next Steps – Robotic PPS

- **Smarter uses of the Robotic positioners**
 - ✓ Haptic motions
 - ✓ Smart trajectories
 - ✓ Vision guidance
- **Add tracking software to enlarge useable work envelopes**
- **Improved calibration methods**
- **Integrate the PPS better with PAS and Control systems**



2-4. Patient Positioning System (3)

Volumetric Image Registration (CBCT)



2-5. Trend of Proton Therapy Facility

- Particle therapy is **in the midst of a remarkable transition**
- During the next decade, important advances in **proton therapy treatment delivery, treatment planning, and quality assurance systems** will be made.
- **IMPT** is becoming **routine treatment** in PT facilities
- **More hospital-based, state-of-art of proton facilities** will be built and increasing PT patients.

On going technique of Proton therapy

Flash therapy; Ultra high dose rate (~ 40 Gy/s)

Spatially Fractionated RT

Flash therapy

- ❖ Described by Town et al. (1967) first
- ❖ Applied to tumors first (Favaudon & Vozenin et al. 2015)
- ❖ Bourhis et al. (2019): first patient treatment

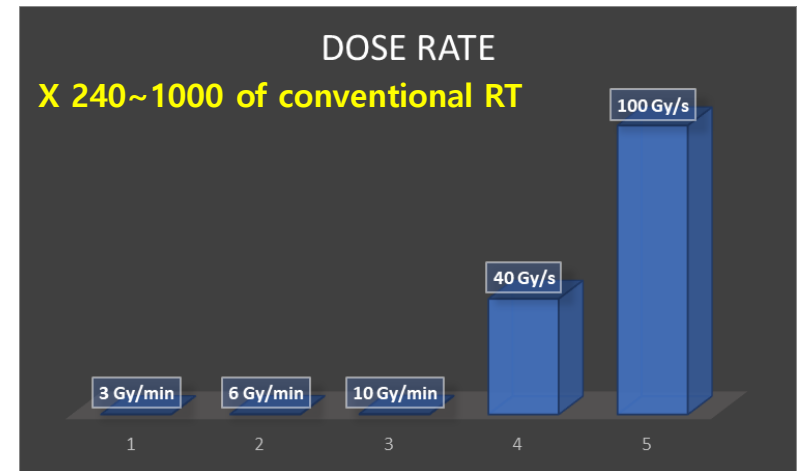


(skin of a pig, 5.6 MeV ; @ 9 months post-RT)

Vozenin et al 2019 ; Bourhis et al 2019

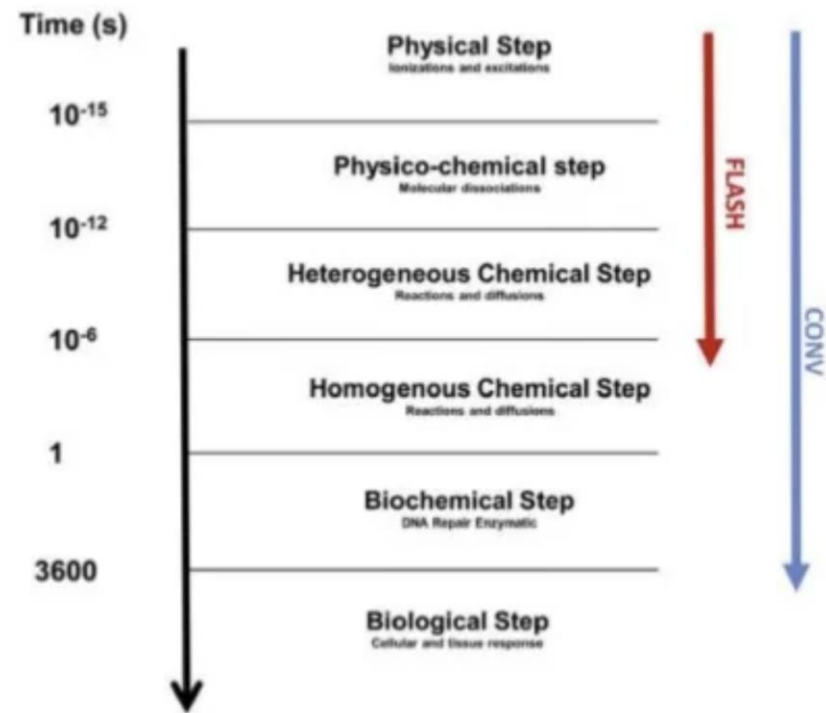
Physical parameters: FLASH Effects

- Dose rate: >40 Gray/sec (possible); >100-150 Gray/sec (likely)
- Reproducible effect
 - Dose / pulse (> 1.5 Gy & few pulses)
 - Dose rate in the pulse ($\geq 10^6$ Gy /s)
 - Overall time (< 100 ms)
- Dose/fraction
 - Begins to show up at >10 Gray/fraction
 - No dose limiting effect observed in animal models between 25-41 Gray
- Radiation type
 - Most reproducible with electrons
 - Ongoing work on X-rays and protons



Biological effect

- Complete oxygen depletion in cells: well oxygenated normal tissues are spared
- Difference in redox biology of the oxygen metabolism
- Different immune effect (less cytokine release: less normal tissue damage)
- Differential gene expression induced by FLASH



Spatially Fractionated therapy

(Grid, Microbeam, Minibeam ...)

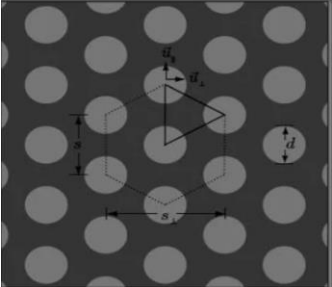
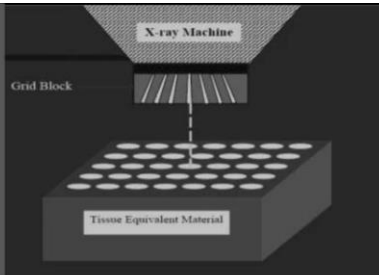
- ❖ Kohler (1909): radiation through a “perforated screen” creating an effect similar to treatment with multiple small pencil beam
- ❖ Liverson (1933): used this technique for the successful treatment of deep seated cancers

SFRT

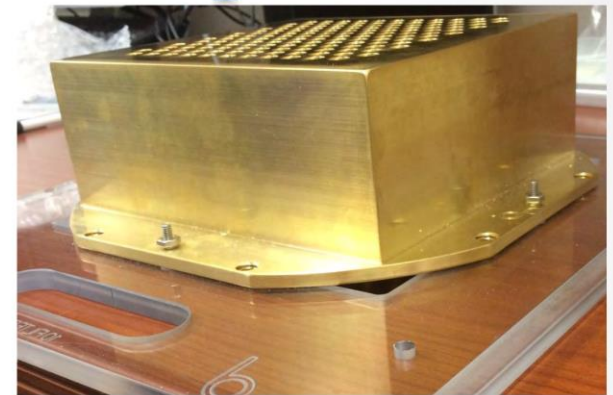
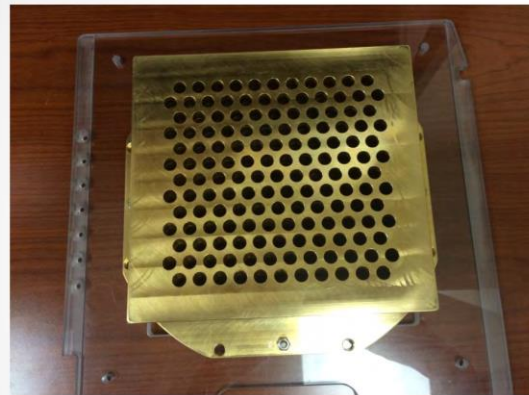
Delivery of radiation in clusters of small areas without producing prohibitive normal tissue damage to the skin and subcutaneous tissue

Small volume of skin could safely tolerate high doses of radiation

Grid is an 8 cm thick lead block containing cylindrical holes. The central axis of each hole was drilled to match the divergence of the radiation from its central axis.



Holes were arranged in a hexagonal array. At the isocentre, they projected 1.3 cm diameter circles separated by 1.8 cm.

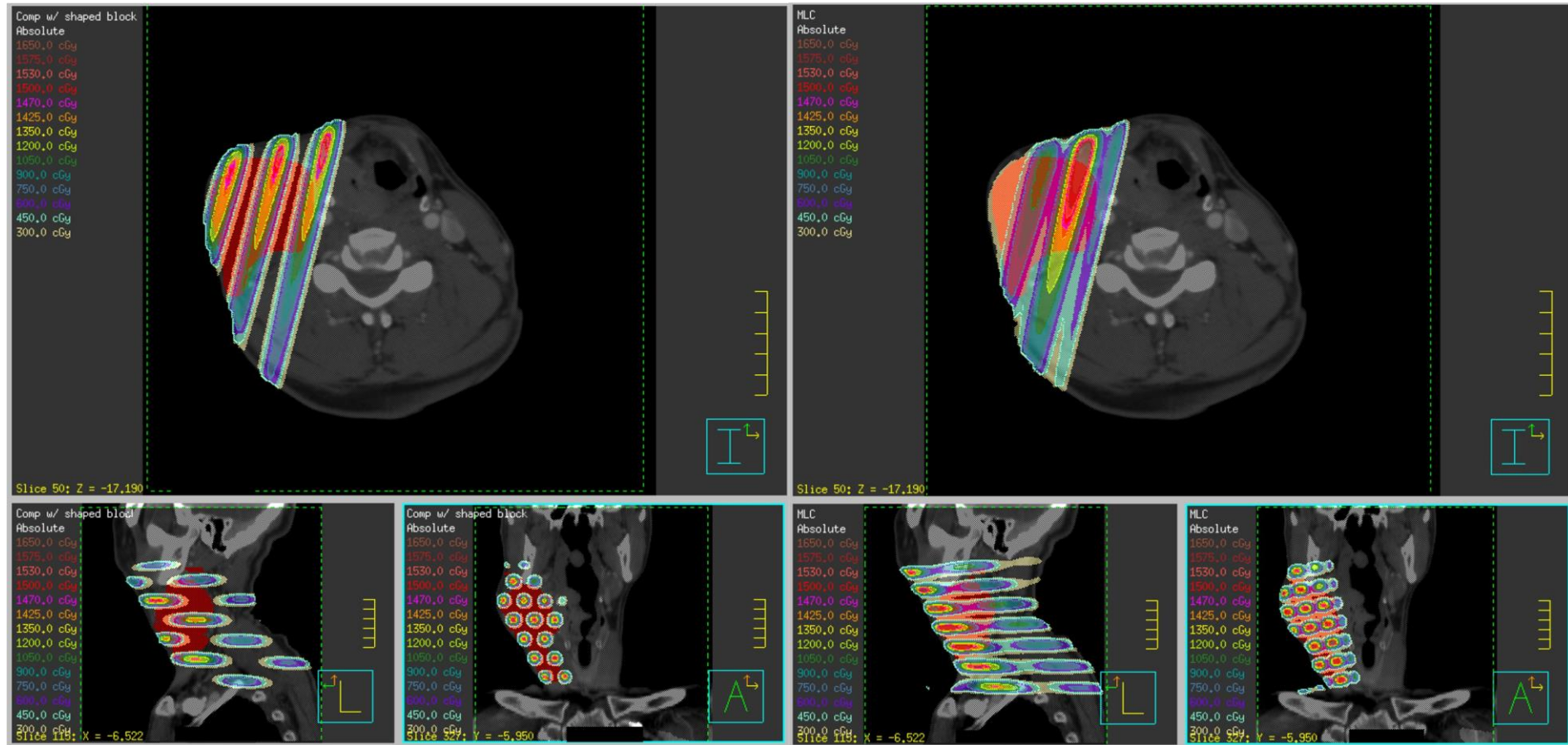


- Constructed from a block of brass by .decimal (.decimal Inc., Sanford, FL)
- Approximately 7.62cm thick and weighs 15.8kg
- Hole centers are 2.11 cm from center to center and 1.43cm in diameter at isocenter

SFRT

- Exact biological response is not fully known
- Believed that high single GRID dose incites reoxygenation with a high tumor cell kill
- Reoxygenation can then begin more rapid tumor response and higher efficiency of a traditional external beam fractionation following GRID
- Bystander effect may also contribute to effectiveness of GRID
- High direct cell kill
- Can cause indirect cell kill of nearby cells due to excretion of cytokines upon death of the nearby cells

SFRT



Grid Compensator

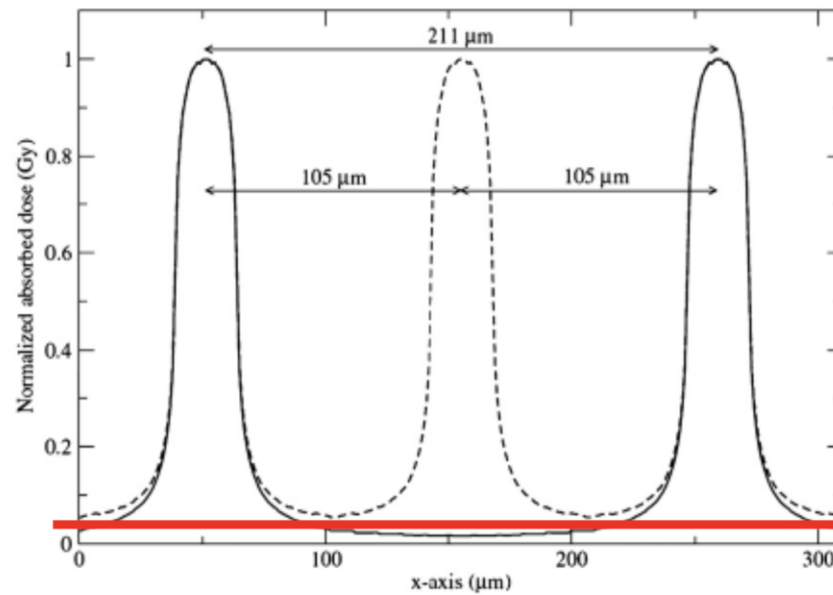
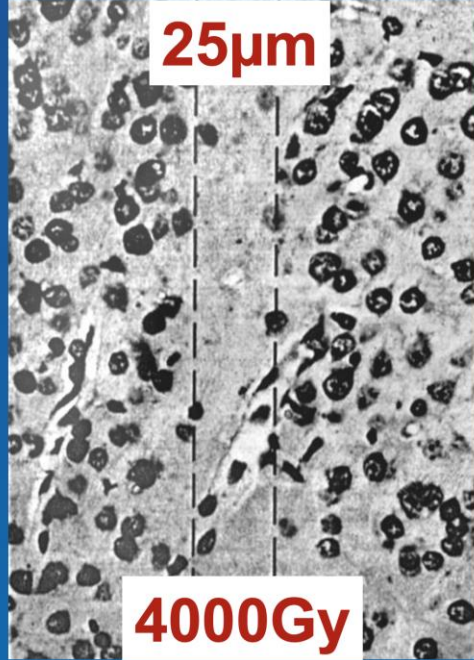
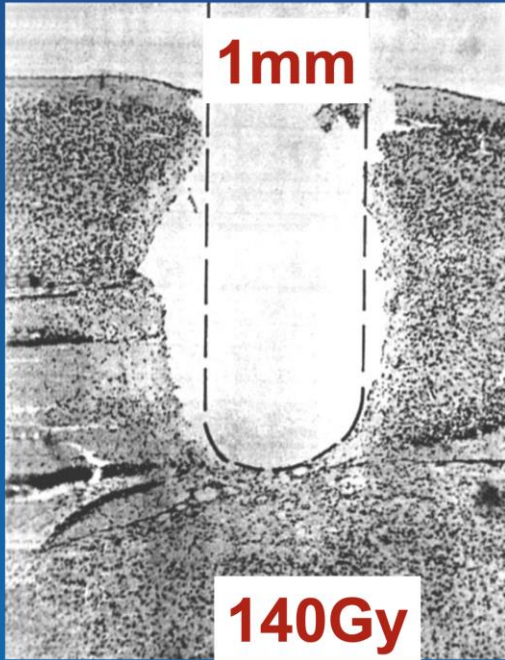
MLC based

(4) Buckey, Courtney et al. Evaluation of a commercially-available block for spatially fractionated radiation therapy. **Journal of Applied Clinical Medical Physics**, [S.l.], v. 11, n. 3, apr. 2010. ISSN 15269914.

SFRT, micro-beam

Dose volume effect

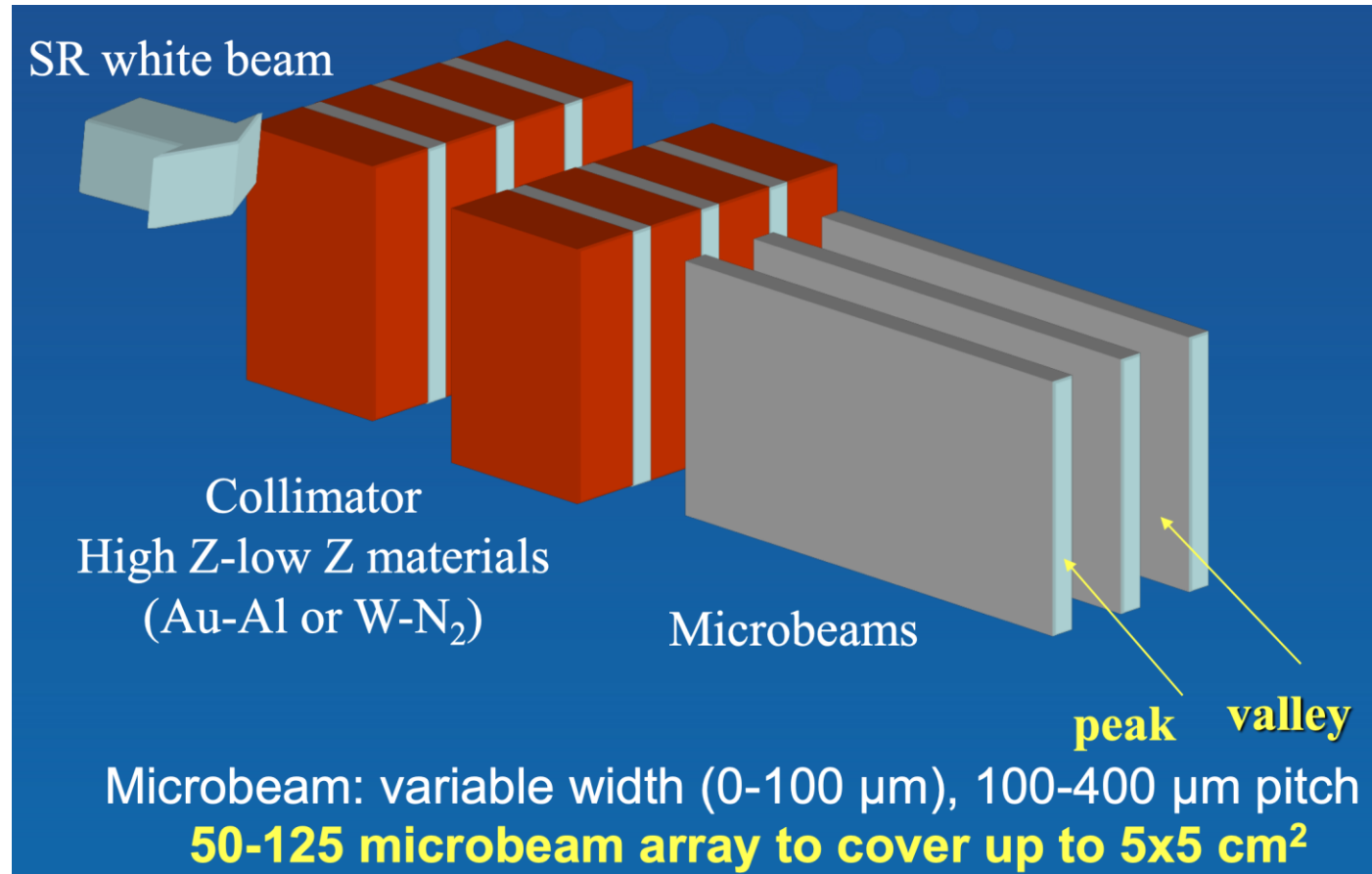
Mouse brain, visual cortex



Tissue tolerance
threshold dose for
healthy tissue
homogeneous
irradiation

The dose in the valleys that creates a dose offset in the tissues, has to be below the tolerance threshold dose

SFRT, micro $\rightarrow$ mini-beam

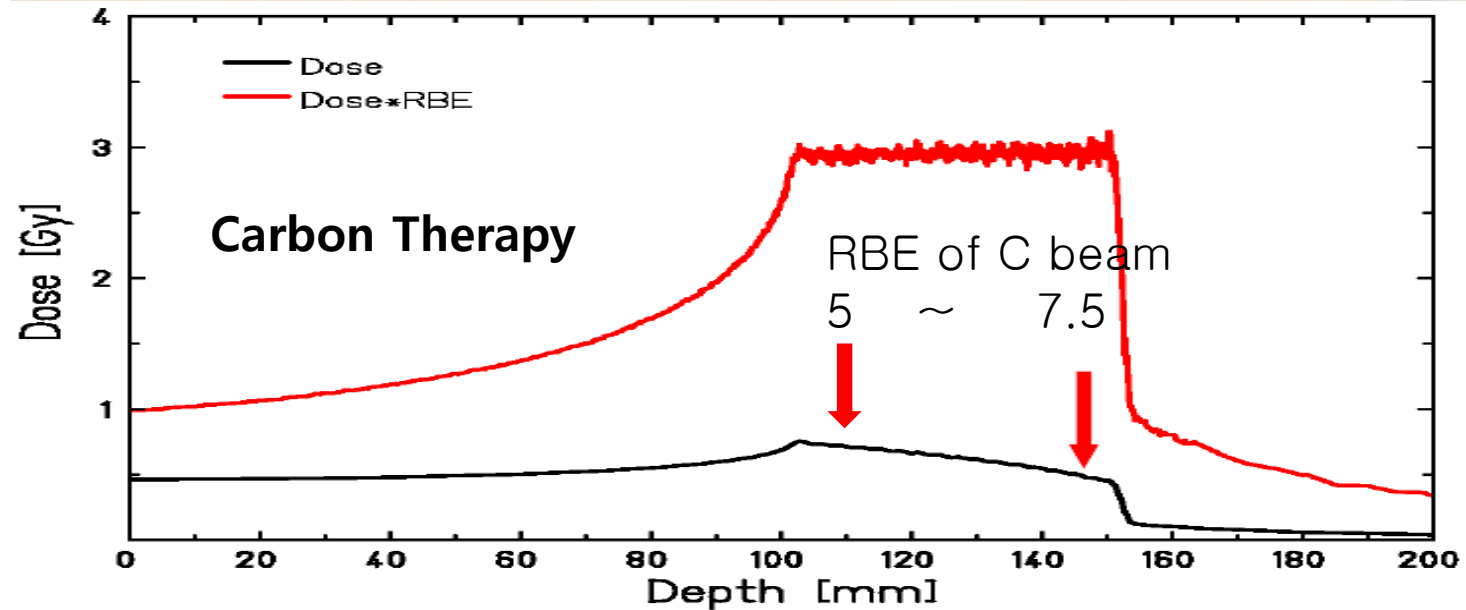
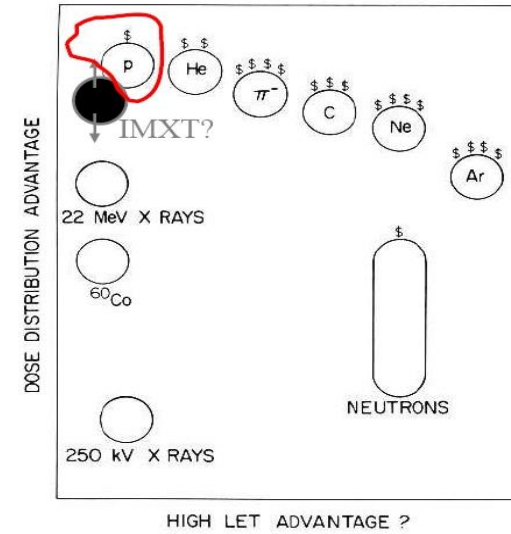
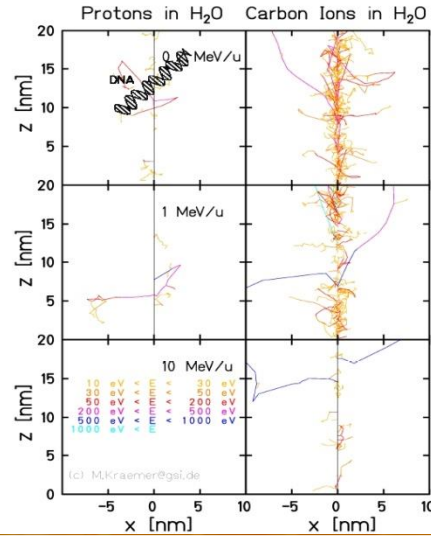


~ mm

Mini-beam

Carbon Therapy

RBE consideration for heavy ions

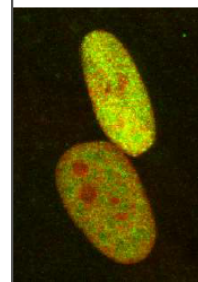


Carbon Therapy Advantages

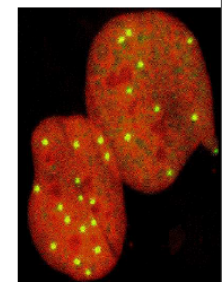
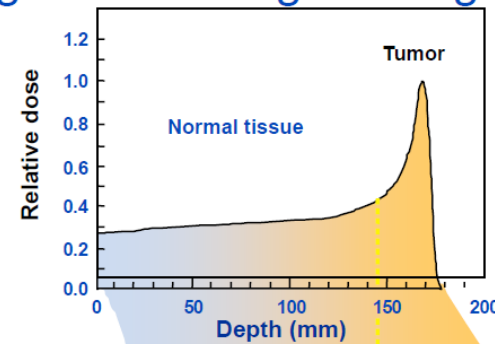
Physical advantages of heavier ions vs. protons

- Reduced angular scattering: sharper penumbra
- Reduced range straggling: sharper distal fall-off
- Better targeting due to better in-vivo monitoring
- There is a whole variety of heavy ions

Biological Advantages of high LET RT



Low LET dose



Carbon tracks
in nucleus

Durante, Loeffler,
*Nature Rev Clin
Oncol* 2010

	Normal tissue	Tumor
Energy	high	low
LET	low	high
Dose	low	high
RBE	≈ 1	> 1
OER	≈ 3	< 3

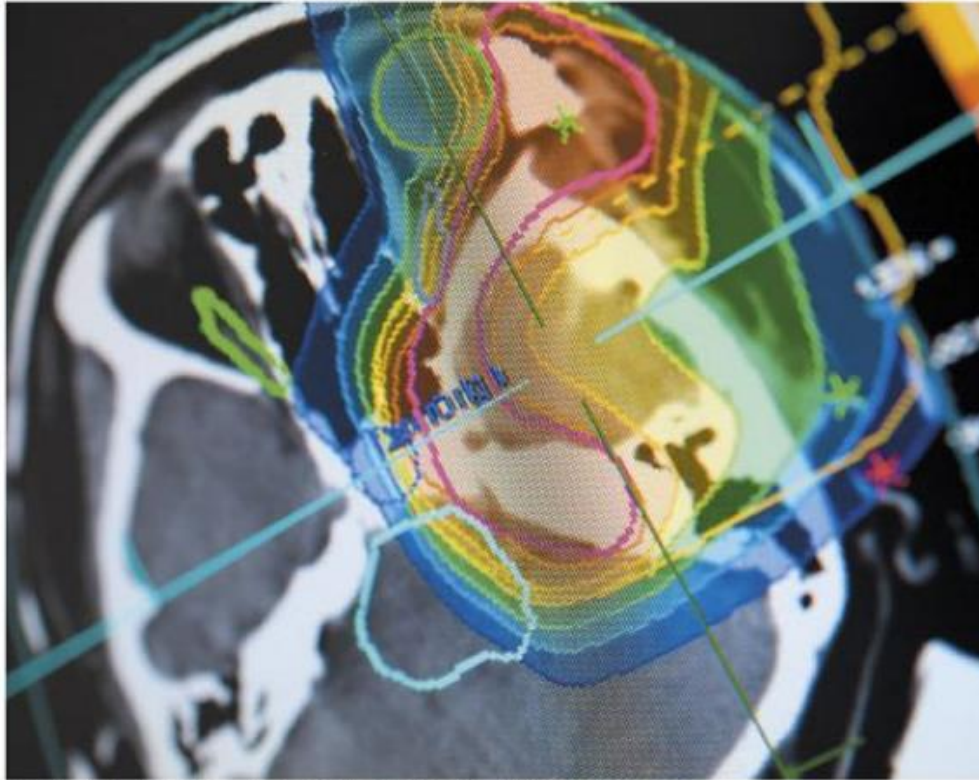
Tumor dose $\gg$ normal tissue

Effective for radioresistant tumors

Effective in hypoxic tumor cells

TECHNOLOGY FEATURE SHARP SHOOTERS

Beams of charged particles can treat cancer more safely and effectively than X-rays. Physicists and biomedical researchers are working to refine the technology for wider use.



A computed-tomography scan shows a tumour and the ion-beam dosage that will be used to treat it.

BY VIVIEN MARX

Clinicians attack cancer with many types of weapon, ranging from scalpels to physically remove all or most of a tumour to drugs that kill the tumour cells where they are. In about half of people with cancer, doctors go after the malignant cells with ionizing radiation.

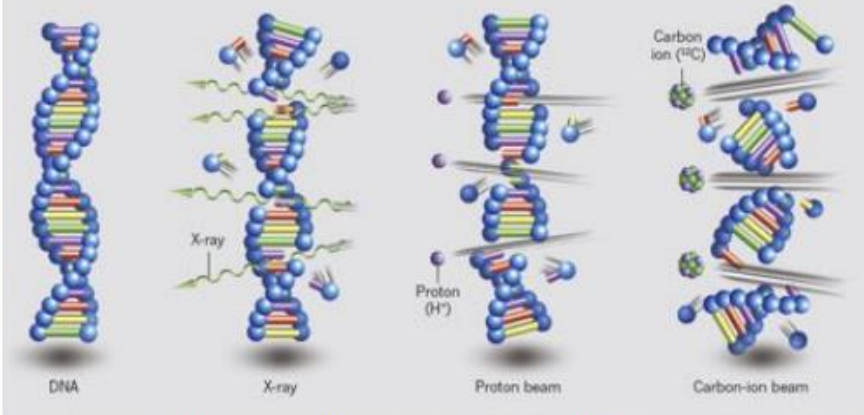
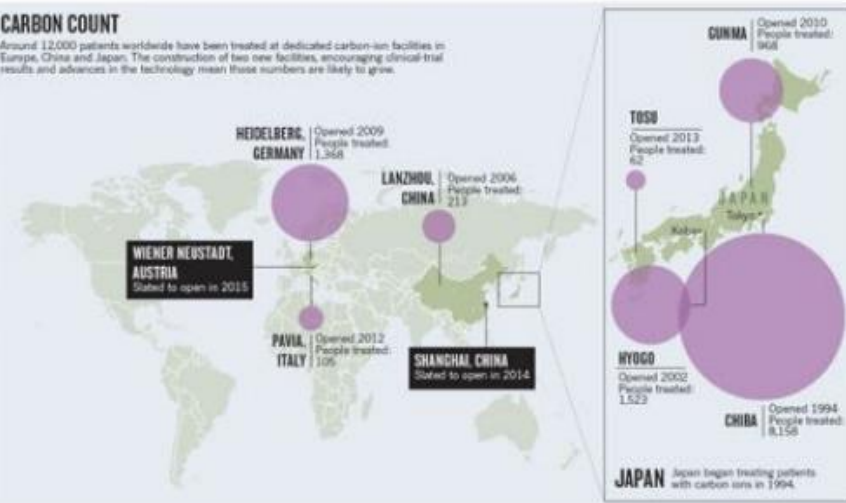
along their path through the body — damaging healthy cells as they go — clinicians and researchers are increasingly paying attention to beams that use charged particles such as protons and carbon ions¹. Charged particles can deposit most of their lethal energy mainly at the tumour site, largely sparing the healthy tissue. Protons are slightly more lethal to cancer cells than X-rays, and carbon ions seem a deadly. 100,000 people have

received proton treatments for cancer. Japan, China, Germany and Italy have built ion-beam facilities that have treated some 12,000 patients with carbon ions, the majority in Japan and Germany (see 'Carbon count').

Carbon ions are heavier than protons, so the facilities to deliver them are pricier. The charged-particle facilities in Germany and Japan cost between US\$130 million and \$200 million each to build. Nonetheless, there has been a spike in research and

CARBON COUNT

Around 12,000 patients worldwide have been treated at dedicated carbon-ion facilities in Europe, China and Japan. The construction of two new facilities, encouraging clinical-trial results and advances in the technology mean these numbers are likely to grow.



Radiation can kill cancer cells by damaging their DNA.

X-rays can hit or miss.

Protons are slightly more lethal to cancer cells than X-rays.

Carbon ions are around 2–3 times as damaging as X-rays.

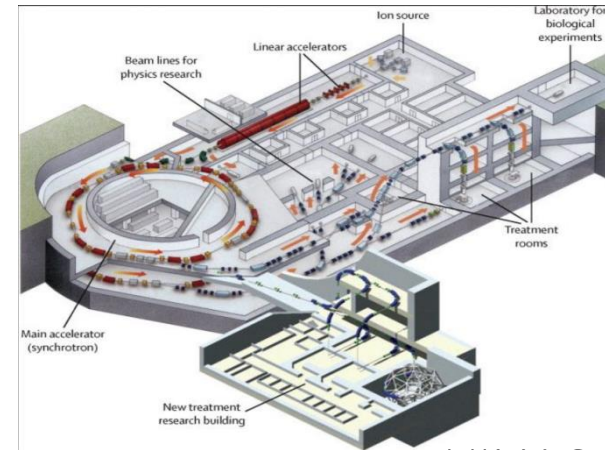


Cancer treatment: Sharp shooters,
Nature 508, 133–138 (03 April 2014)

Example of Carbon-Beam Therapy Center



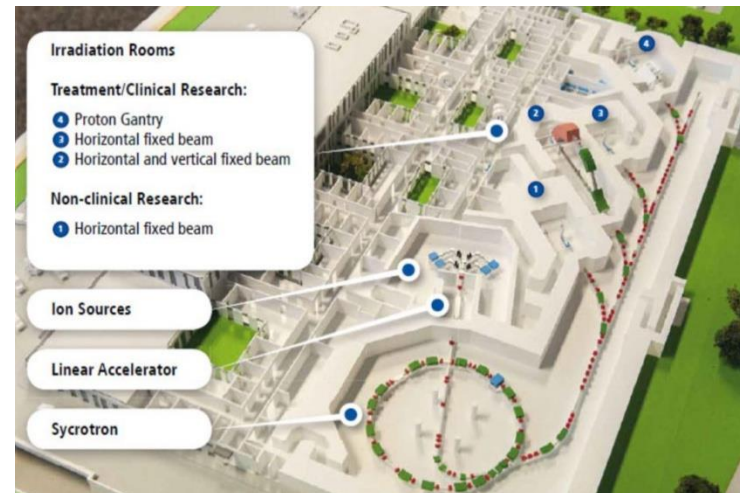
HIT



HIMAC-NIRS



HIBMC



MedAustron

World Carbon-Beam Therapy Center

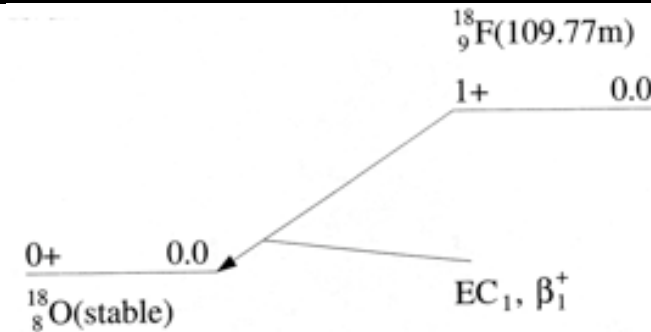
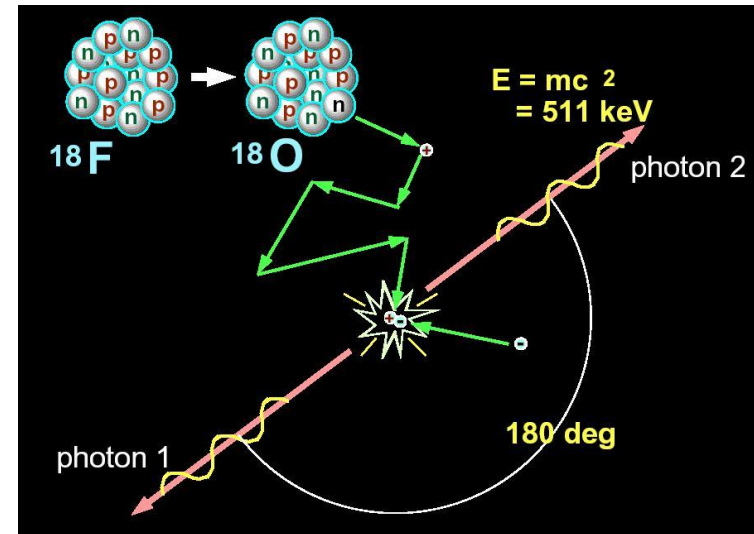
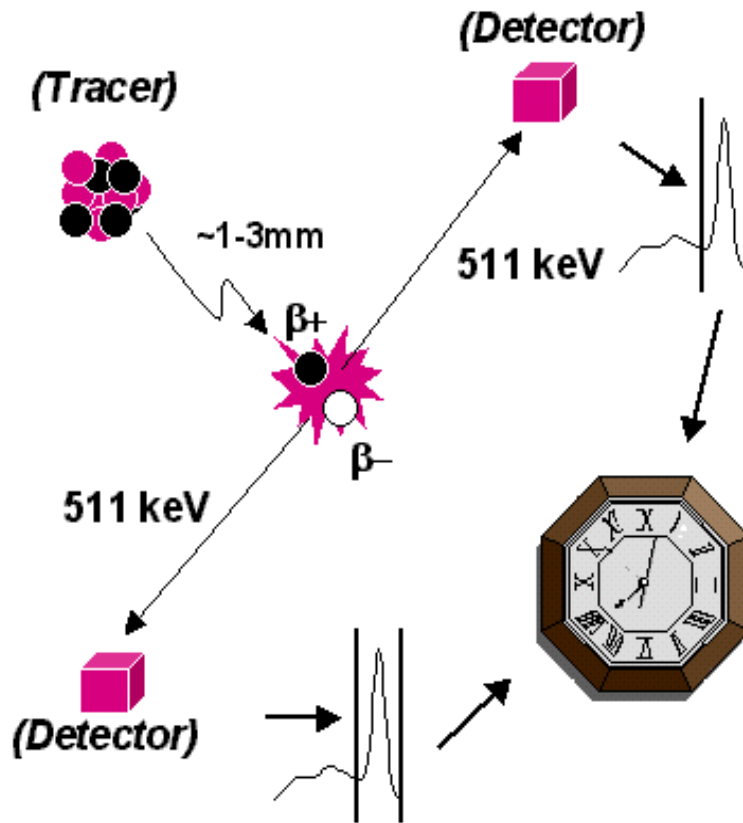
	COUNTRY	WHO, WHERE	PARTICLE	S/C/SC* MAX. ENERGY (MeV)	BEAM DIRECTIONS	START OF TREATMENT
1	Austria	MedAustron, Wiener Neustadt	C-ion	S 403/u	2 horiz. and 1 vertical fixed beam**	2019
2	China	SPHIC, Shanghai	C-ion	S 430/u	3 fixed beams**	2014
2	China	Heavy Ion Cancer Treatment Center,	C-ion	S 400/u	4 fixed beams**	2019
2	Germany	HIT, Heidelberg	C-ion	S 430/u	2 fixed beams, 1 gantry**	2009, 2012
2	Germany	MIT, Marburg	C-ion	S 430/u	3 horiz., 1 45deg. fixed beams**	2015
1	Italy	CNAO, Pavia	C-ion	S 480/u	3 horiz., 1 vertical, fixed beams	2012
7	Japan	HIMAC, QST, Chiba	C-ion	S 800/u	horiz.***, vertical***, fixed beams, 1 gantry	1994, 2017
7	Japan	HIBMC, Hyogo	C-ion	S 320/u	horiz., vertical, fixed beams	2002
7	Japan	GHMC, Gunma	C-ion	S 400/u	3 horiz., 1 vertical, fixed beams	2010
7	Japan	SAGA-HIMAT, Tosu	C-ion	S 400/u	3 horiz., vertical, 45 deg., fixed beams	2013
7	Japan	i-Rock Kanagawa Cancer Center, Yokohama	C-ion	S 430/u	4 horiz., 2 vertical, fixed beams	2015
7	Japan	Osaka Heavy Ion Therapy Center, Osaka	C-ion	S 430/u	3 fixed beams, 6 ports**	2018
7	Japan	East Japan HIC, Yamagata University Hospital, Yamagata	C-ion	S 430/u	1 SC gantry**, 1 horiz. & vertical fixed beam	2021

World Carbon-Beam Therapy Center (under construction)

COUNTRY	WHO, WHERE	PARTICLE(S)	MAX. ENERGY (MeV) ACCELERATOR TYPE (VENDOR)*	BEAM DIRECTIONS	NO. OF TREATMENT ROOMS	START OF TREATMENT PLANNED
China	HITFil at IMP, Lanzhou, Gansu	C-ion	400/u synchrotron (?)	4 horiz, vertical, oblique, fixed beams	4	2022?
France	ARCHADE, Caen	C-ion	400/u cyclotron (IBA)	1 fixed beam (r&d)	1	2023
South Korea	Seoul National University Hospital, Busan	C-ion, He-ion	430/u for C, 230 MeV/u for He synchrotron (Toshiba)	1 gantry, 1 horiz. fixed beam	2	2025
South Korea	Yonsei University Hospital, Seoul	C-ion	430/u, synchrotron (Toshiba)	2 gantries, 1 horiz. fixed beam	3	2022
Taiwan	Taipei Veterans General Hospital, Taipei	C-ion	430/u synchrotron (Hitachi)	2 vertical and 2 horizontal fixed beams	2	2021/2022
USA	Mayo Carbon Ion Therapy Center, Jacksonville, FL.	p, C-ion	250, 430/u, synchrotron (Hitachi)	1 gantry (p), 2-3 fixed beams (C-ion)	3-4	2025+

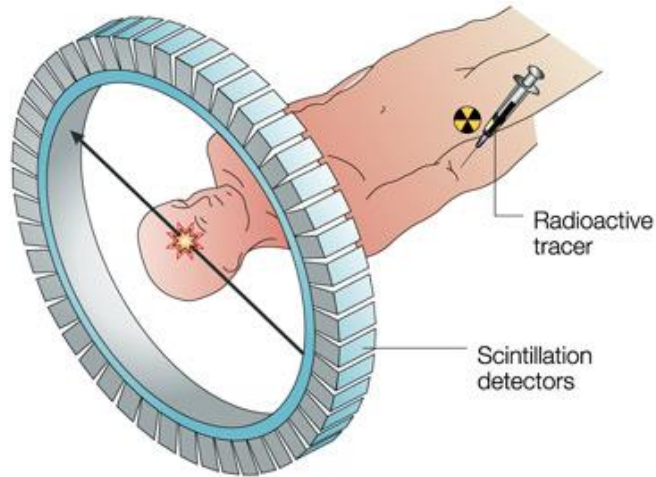
Positron Emission Tomography?

Positron Annihilation

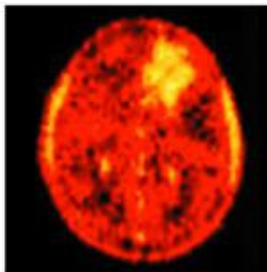


Clinical Use of PET – Functional Imaging

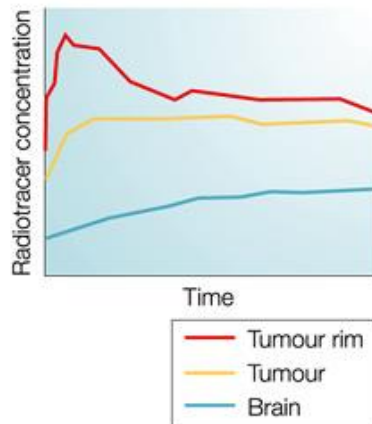
a Patient in a scanner



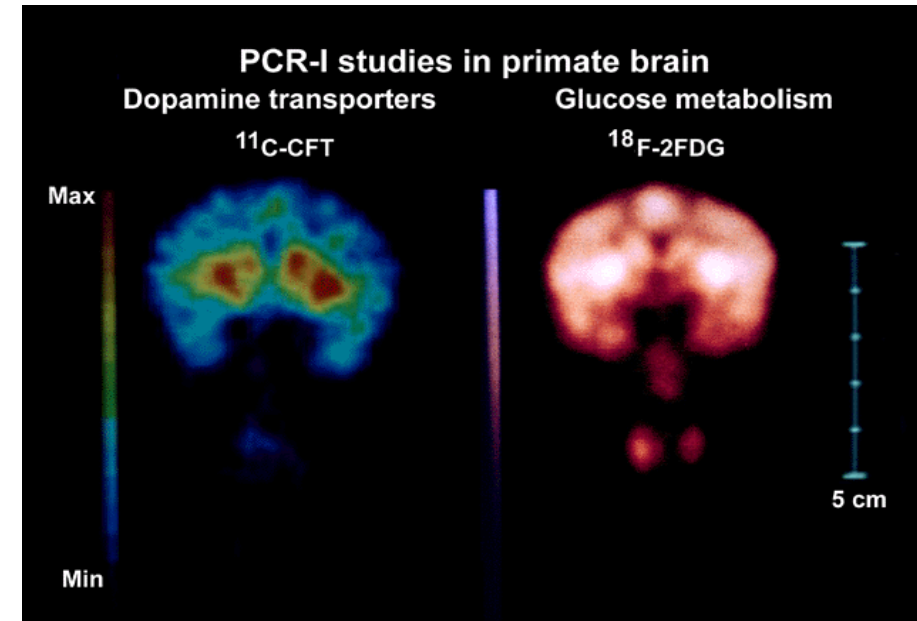
b PET image



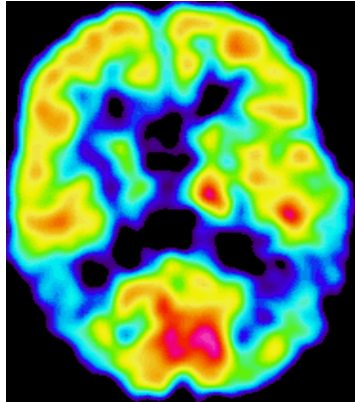
c Radiotracer concentration over time



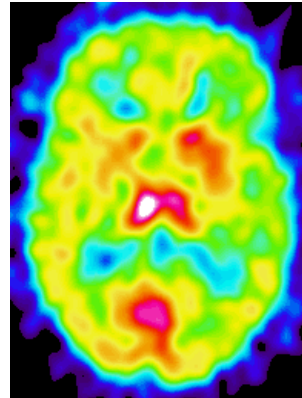
Single ring positron emission tomography (1985)



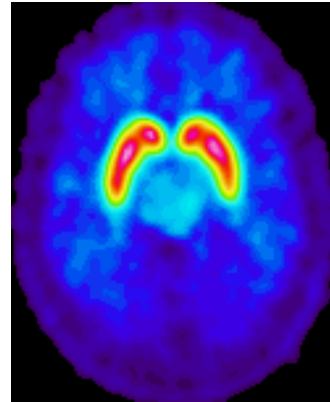
Example of PET imaging



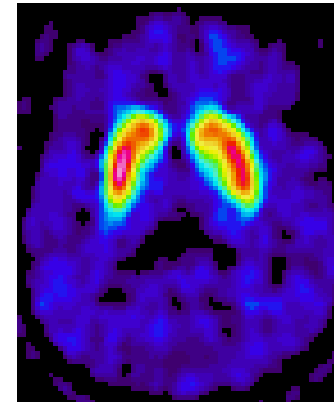
Glucose metabolism
 ^{18}F Fluorodeoxyglucose



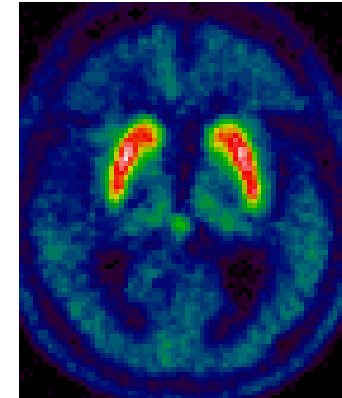
Inflammation
 ^{11}C D-Deprenyl



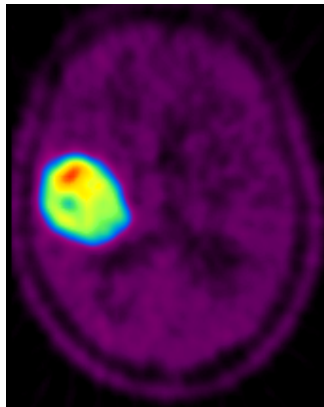
Dopamine reuptake
 ^{11}C BCIT



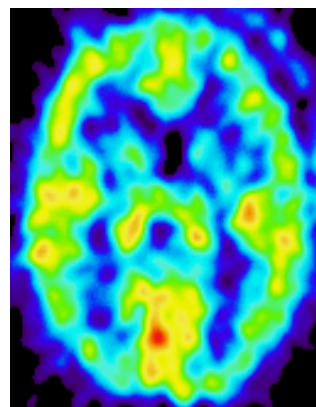
D2-receptors
 ^{11}C Raclopride



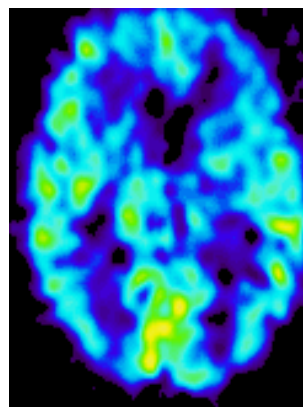
Dopamine synthesis
 ^{18}F Dopa



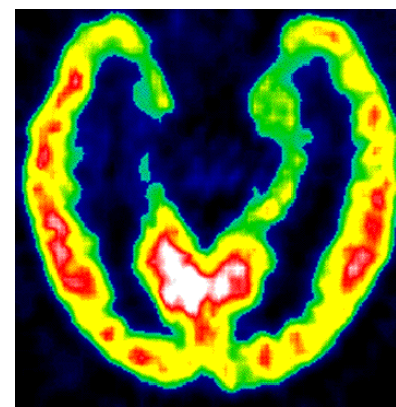
Amino acid uptake
 ^{11}C Methionin



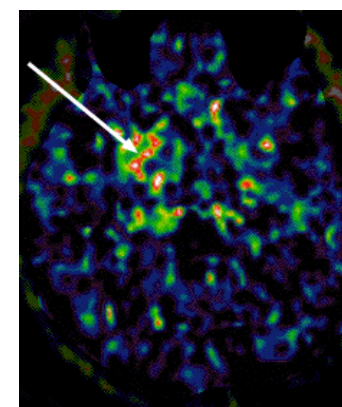
Blood flow
 ^{15}O Water



Oxygen Consumption
 ^{15}O Oxygen



Central BZ-receptors
 ^{11}C Flumazenil

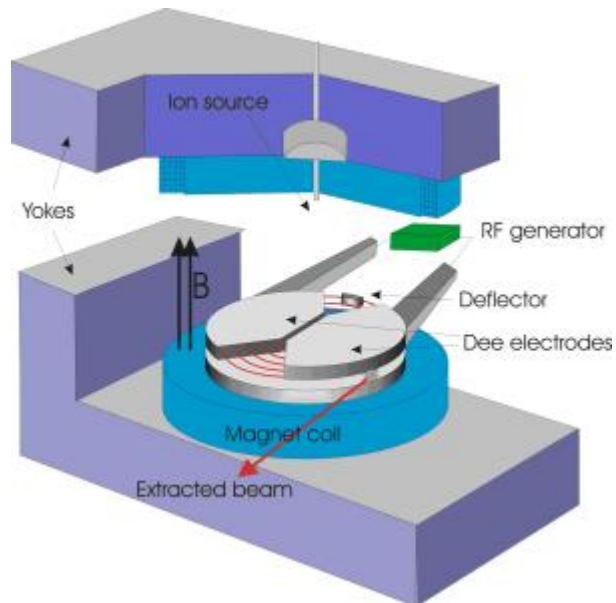


Microglia activation
 ^{11}C PK11195

Radio-nuclides Production using Particle Accelerators

Nuclide	Half-life
C-11	20.3 min.
N-13	10 min.
O-15	124 sec.
F-18	110 min.
Rb-82	75 sec.

Cyclotron



A Course of Radiation Therapy

Radiography

- In 1895, Wilhelm Conrad Röntgen discovered new kinds of ray emitted by a gas discharge tube that could blacken photographic film.
- The first radiograph.



Rontgen Museum, Germany

2) 방사선치료의 역사

1895 Roentgen – X-ray

1898 Curie – Radium (brachytherapy)

1900 Becquerel – radiobiology

1922 Clinical approach(larynx cancer)

1934 Fractionated radiation therapy

1970- Computer Treatment Planning System

1980- 3D Conformal Radiation Therapy (CRT)

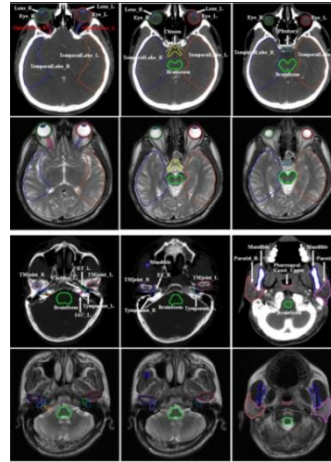
1990- Intensity Modulated Radiation Therapy (IMRT)

2000- Image Guided Radiation Therapy (IGRT)

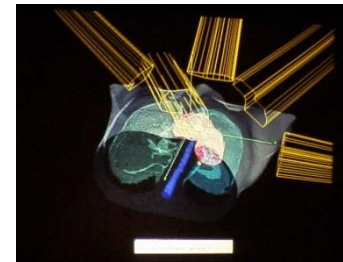
Radiation Treatment



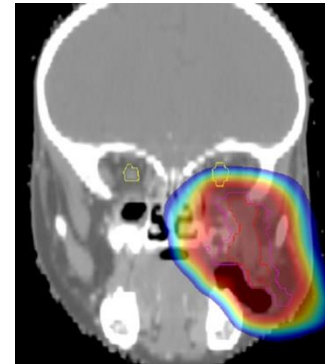
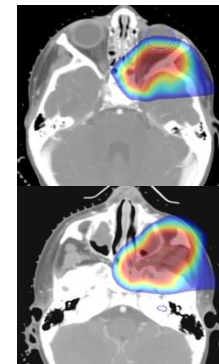
CT simulation



Organs & Tumors
Segmentation

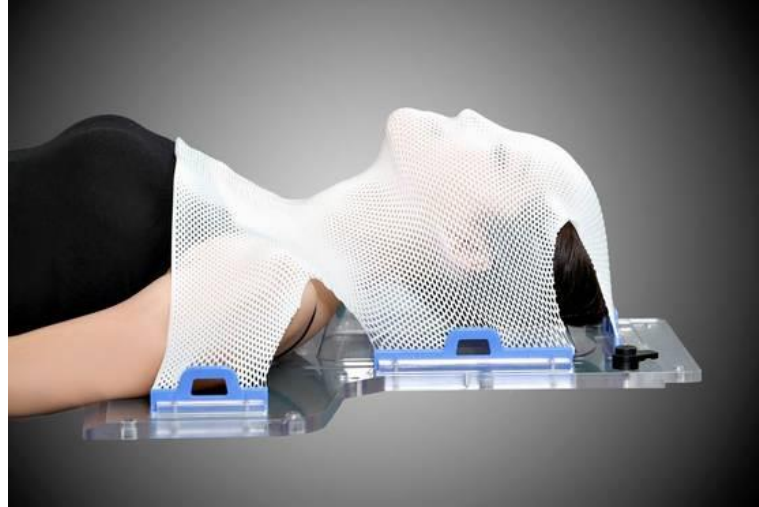


Treatment
Planning



Radiation Treatment & Radiation Dose Distribution on Patient Body

CT simulation



US, MR, PET, ...

❖ Usefulness of CT

- (a) **delineation** of target volume and the surrounding structures in relation to the external contour → most important
 - not only crucial for optimizing a treatment technique
 - but also necessary **for accurate calculation of dose** distribution
- (b) providing quantitative data for **tissue heterogeneity corrections**
- ❖ The most severe errors in computing the dose distribution are caused by inaccurate delineation of the geometric outlines of tissue inhomogeneities rather than inaccurate relative electron density for the inhomogeneity
 - However, **severe dose gradient region** in the direction of the beam → greater precision in the **inhomogeneity outline** and **electron density** are required
 - For electron beam therapy, and in regions where electronic equilibrium is not established in high-energy photon beam
 - **Pixel-by-pixel correction method**
 - In the case of **lung correction**, dose calculation algorithms **based on electron transport** (convolution/superposition or Monte Carlo) are necessary to provide accuracy of better than **5%**

Segmentation

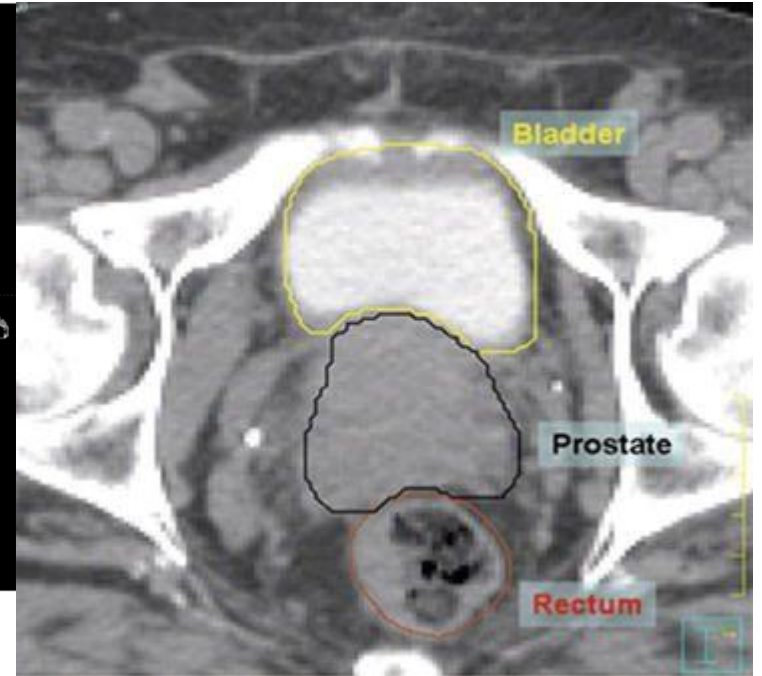
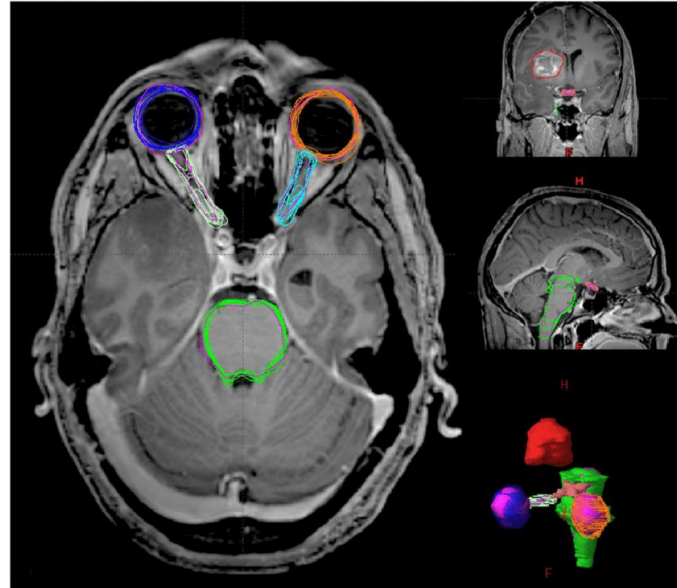
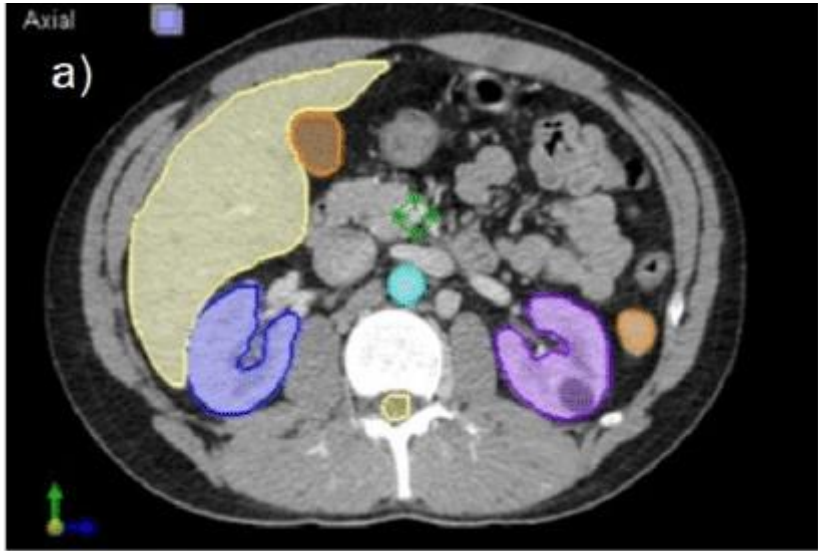
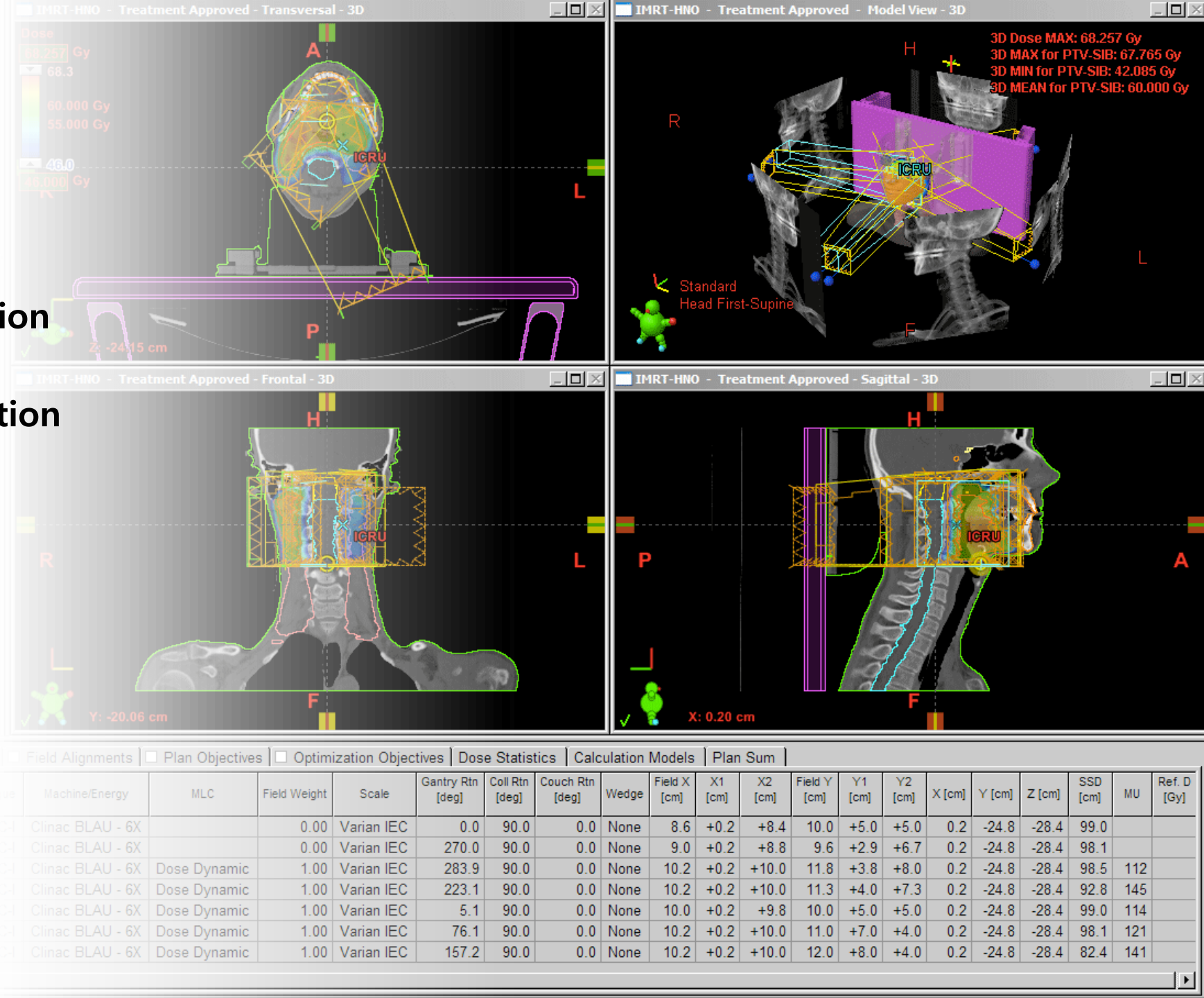


Image registration

Auto segmentation

RT Planning

- Energy fluence Optimization
- MLC movement optimization
- Dose calculation
- Plan Evaluation
- Machine data interface
- Patient Specific Plan QA



Patient Setup



DRR construction

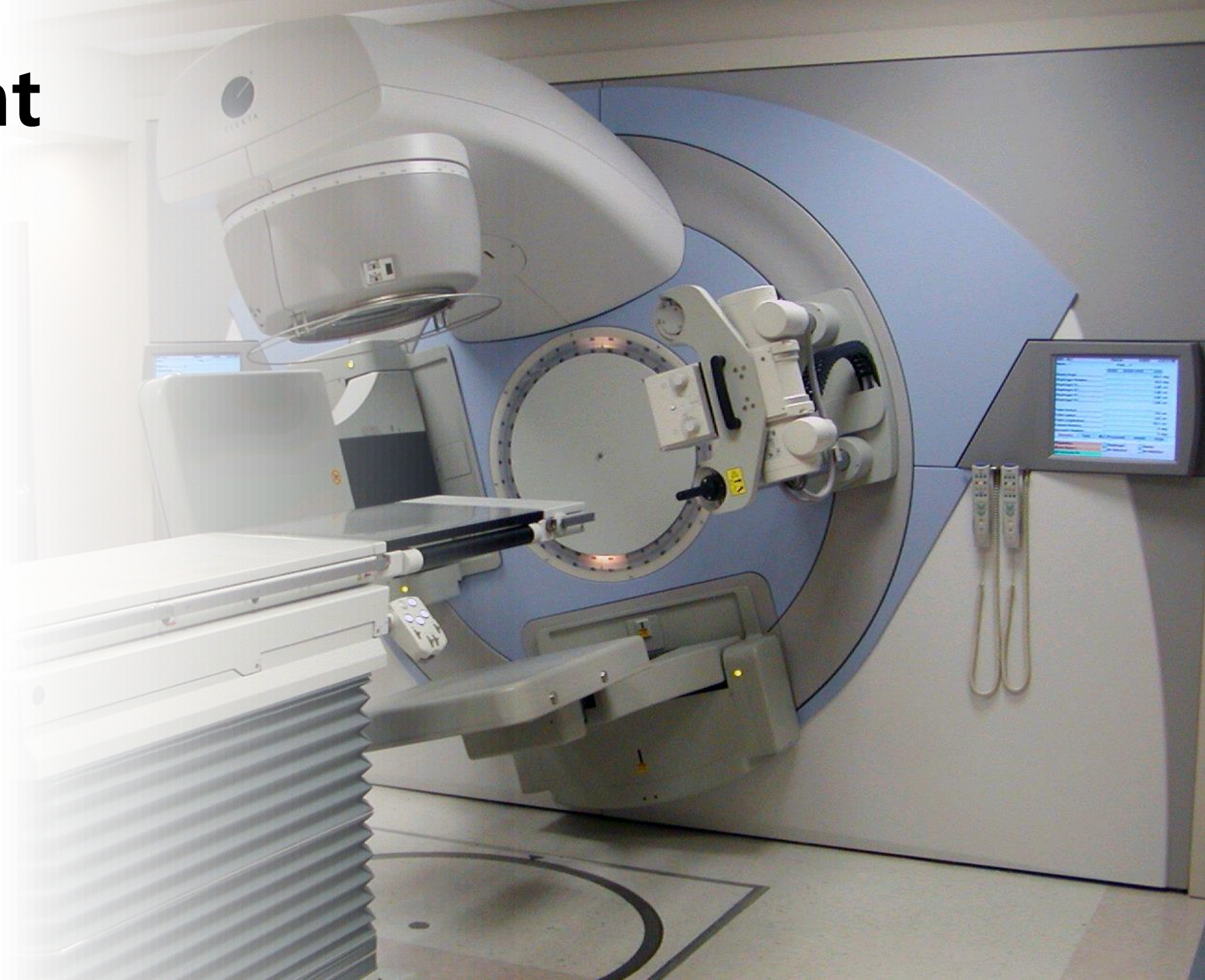
Patient positioning

Patient Immobilization

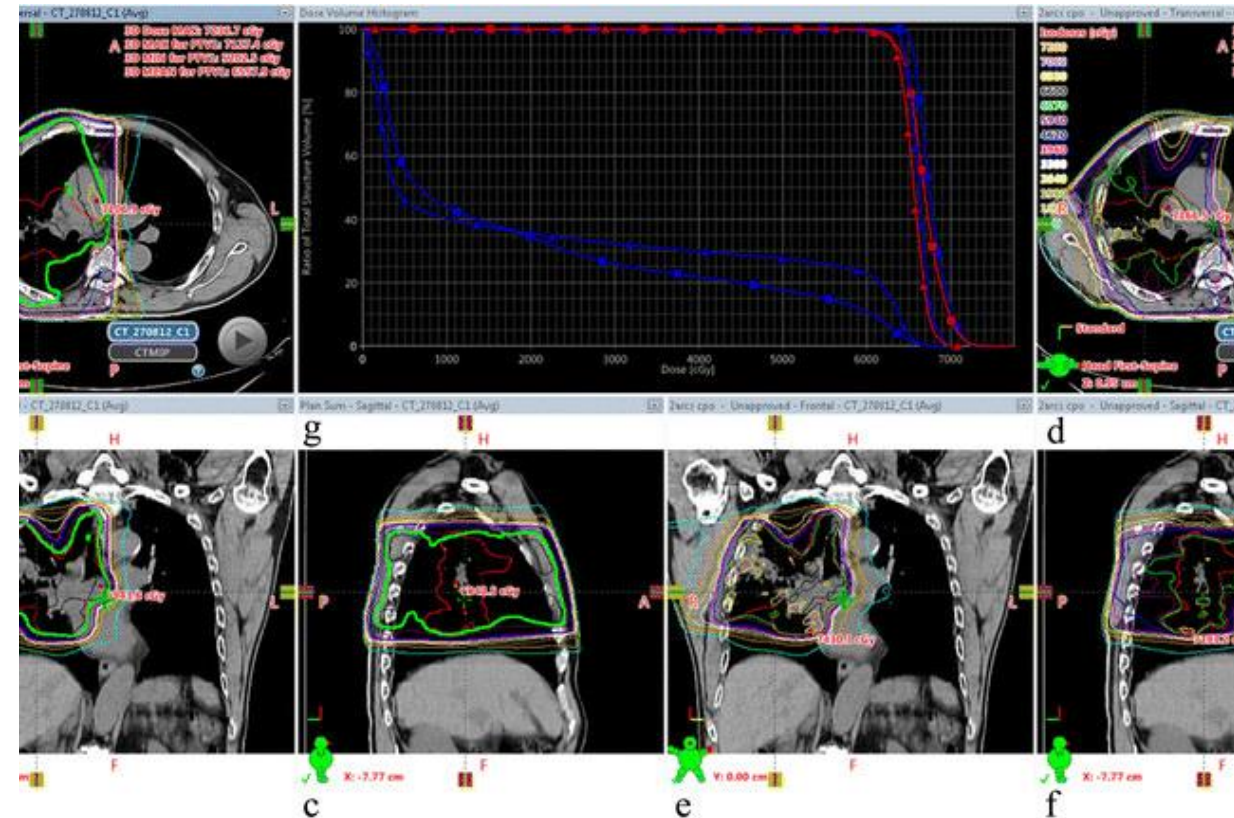
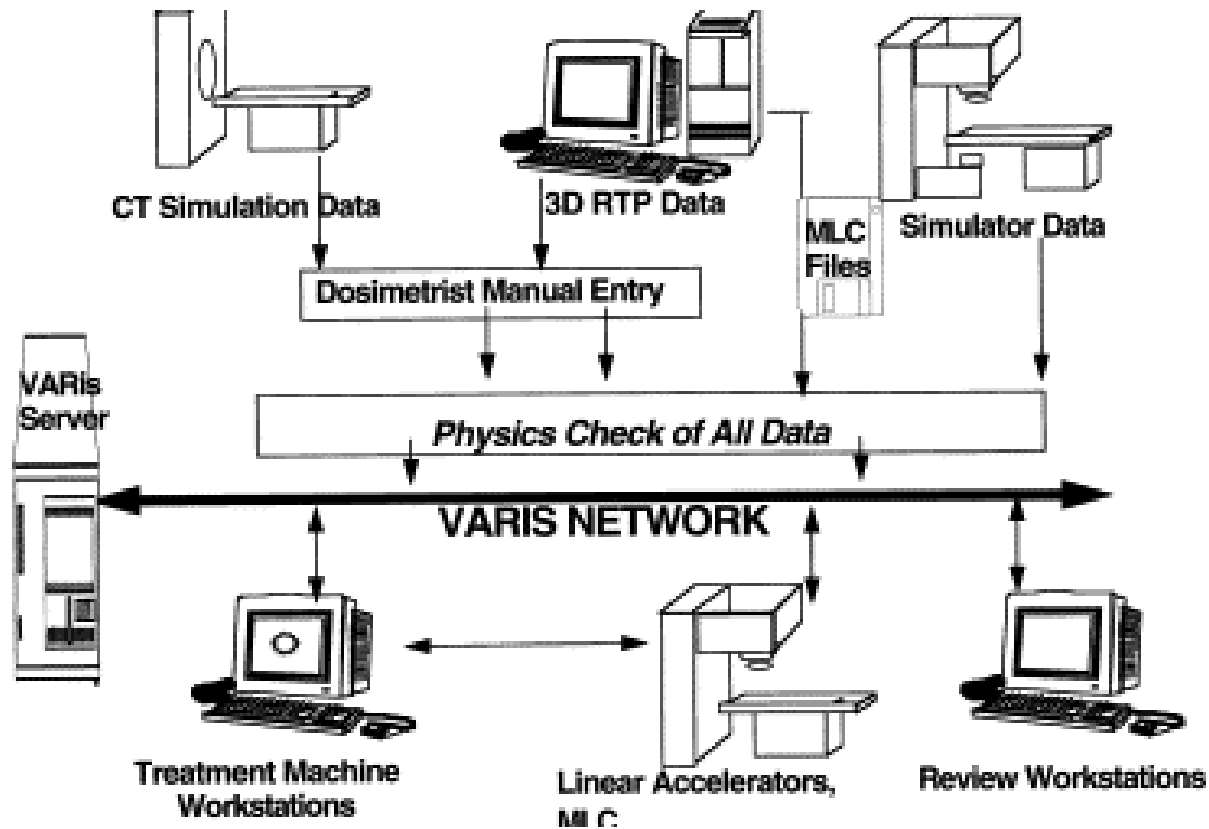


RT Treatment

- Image guidance
- Tumor tracking
- Patient monitoring
- Patient shielding



RT Record and Verify



Quality Assurance

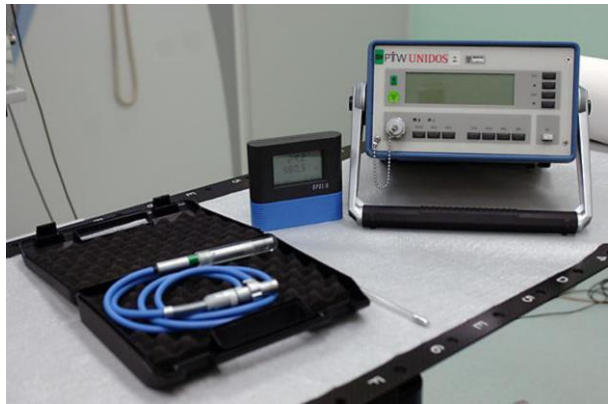
Machine QA



Patient QA



Radiation Dosimetry



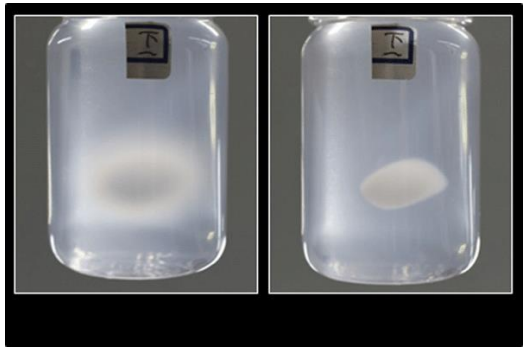
nanoDot slides in and out of the adapter (2D bar code facing front) for read-out in an original microStar reader



Back of open nanoDot carrier with 2D bar code that includes sensitivity code and serial number



Each nanoDot is shipped enclosed in a plastic packet, ready for clinical use



Medical Physics

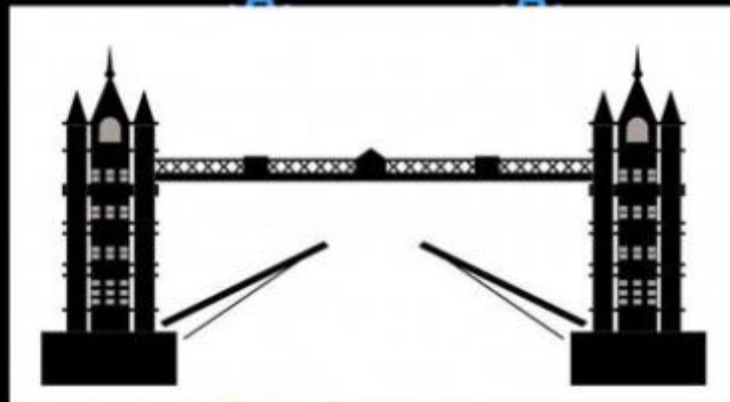


What is Medical Physics?

Application of the concepts and methods of physics to the diagnosis and treatment of human disease

Medical Physicist

Physics



Medicine

Slide adapted from AAPM Medical Physics Education Presentation



**International
Labour
Organization**

Promoting jobs,
protecting people

Medical Physicists (Revised definition provided by International Organisation for Medical Physicists)

Medical Physicists apply knowledge and methodology of science of physics to all aspects of medicine, to conduct research, develop or improve theories and address problems related to diagnosis, treatment, and rehabilitation of human disease. They are directly involved with patients and people with disabilities.

Tasks include –

- (a) Conducting research into human disorders, illnesses and disabilities; investigating biophysical techniques associated with any branch of medicine.
- (b) Conducting specialised examinations of patients and the disabled, improving patient care and clinical services, developing innovative imaging and non-imaging diagnostic

What Medical Physics Covers

Medical Physics is a branch of Applied Physics, pursued by medical physicists, that uses physics principles, methods and techniques in practice and research for the prevention, diagnosis and treatment of human diseases with a specific goal of improving human health and well-being.

Medical physics may further be classified into a number of sub-fields (specialties), including Radiation Oncology Physics, Medical Imaging Physics, Nuclear Medicine Physics, Medical Health Physics (Radiation Protection in Medicine), Non-ionizing Medical Radiation Physics, and Physiological Measurement.

It is also closely linked to neighboring sciences such as Biophysics, Biological Physics, and Health Physics.

First Year		
Semester 1	Course Title	Credit Hrs.
MP-9001	Professional Aspects of Medical Physics	2
BE-7022	Introduction to Biostatistics	3
MP-9041	Radiobiology I	2
MP-9044	Radiation Physics and Dosimetry I	3
MP-9050	Diagnostic Radiological Imaging Physics I	3
MP-9005	Introduction to Clinical Oncology I	1
MP-9092	Seminar: Current Research Topics in Radiological Sciences	1
Total: 15		
Semester 2	Course Title	Credit Hrs.
MP-9041	Radiobiology II	2
MP-9045	Radiation Physics and Dosimetry II	3
MP-9051	Diagnostic Radiological Imaging Physics II	3
MP-9095	Anatomy and Physiology for Radiation Therapy Treatment Planning	3
MP-9072	Radiological Sciences Lab I	2
MP-9011	Clinical Radiation Dosimetry	3
MP-9092	Seminar: Current Research Topics in Radiological Science	1
Total: 17		

Second Year		
Semester 1	Course Title	Credit Hrs.
MP-9096	Radiotherapy Treatment Planning I	2
MP-9013	Hospital Radiation Protection	3
MP-9073	Radiological Sciences Lab II	2
MP-9093	Clinical Medical Physics	4
MP-9092	Seminar: Current Research Topics in Radiological Sciences	1
MP-9099	Research in Radiological Sciences	4
Total 16		
Semester 2	Course Title	Credit Hrs.
MP-9097	Radiotherapy Treatment Planning II	2
MP-9093	Clinical Medical Physics	5
MP-9093	Seminar: Current Research Topics in Radiological Sciences	1
MP-9099	Research in Radiological Sciences	5
Total 15		

Third Year		
Semester 1	Course Title	Credit Hrs.
MP-9015	Clinical Radiation Oncology	1
MP-9061	Clinical Practicum - 3D-CRT	5
MP-9081	QA in Radiation Therapy - Treatment Planning Devices	5
MP-9092	Seminar: Current Research Topics in Radiological Sciences	1
MP-9094	Journal Club	1
MP-9098	Clinical Research in Medical Physics	2
Total 15		
Semester 2	Course Title	Credit Hrs.
MP-9015	Clinical Radiation Oncology	1
MP-9061	Clinical Practicum - IMRT	5
MP-9082	QA in Radiation Therapy - Treatment Delivery Devices	5
MP-9092	Seminar: Current Research Topics in Radiological Sciences	1
MP-9094	Journal Club	1
MP-9098	Clinical Research in Medical Physics	2
Total 15		

Fourth Year		
Semester 1	Course Title	Credit Hrs.
MP-9015	Clinical Radiation Oncology	1
MP-9063	Clinical Practicum - SRS and SBRT	5
MP-9083	QA in Radiation Therapy - Imaging Devices	5
MP-9092	Seminar: Current Research Topics in Radiological Sciences	1
MP-9094	Journal Club	1
MP-9098	Clinical Research in Medical Physics	2
MP-9099	Special Topics in Medical Physics (Elective)	0-2
Total 15-17		
Semester 2	Course Title	Credit Hrs.
MP-9015	Clinical Radiation Oncology	1
MP-9064	Clinical Practicum - Brachytherapy	5
MP-9084	QA in Radiation Therapy - Patient Specific Dosimetry	5
MP-9092	Seminar: Current Research Topics in Radiological Sciences	1
MP-9094	Journal Club	1
MP-9098	Clinical Research in Medical Physics	2
MP-9099	Special Topics in Medical Physics (Elective)	0-2
Total 15-17		

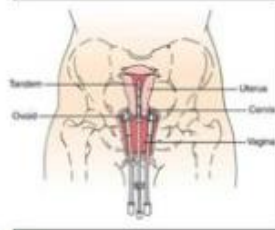
General Areas of Responsibility for Medical Physicist

- Clinical
- Research
- Education
- Regulatory Compliance

Medical Physics Disciplines

- Therapeutic Medical Physics Radiation Oncology
- Diagnostic Medical Physics Radiology
- Nuclear Medical Physics Radiology
- Medical Health Physics Radiation Safety

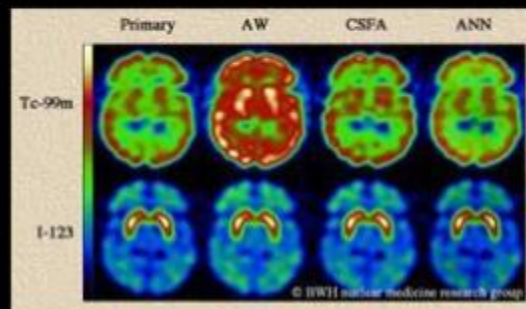
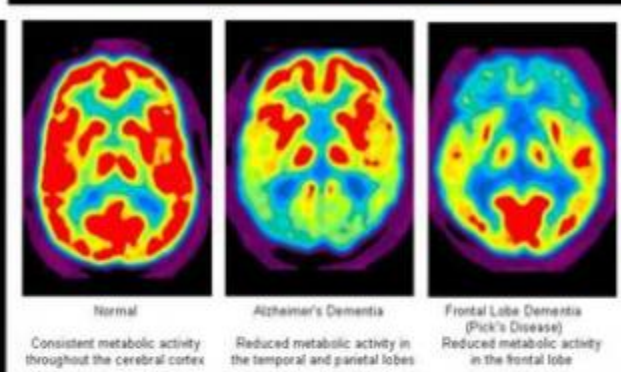
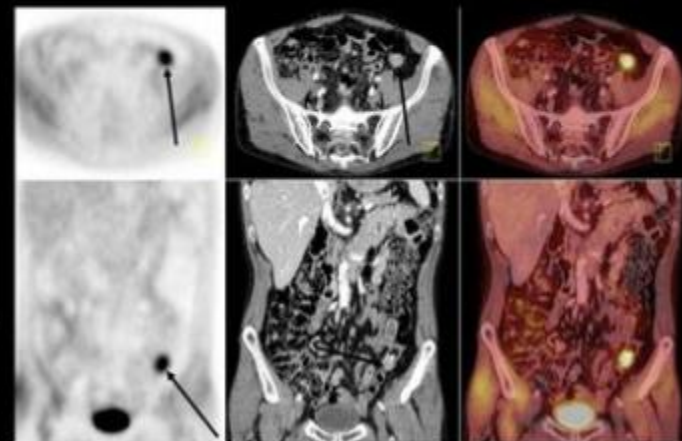
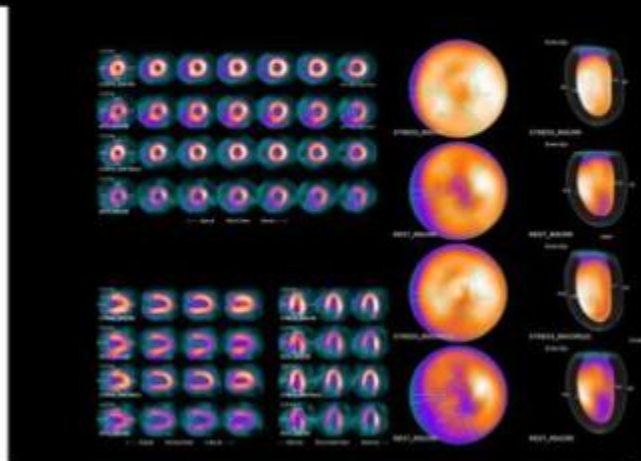
Therapeutic Medical Physics



Diagnostic Medical Physics

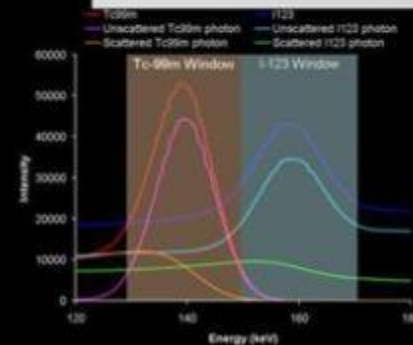


Nuclear Medical Physics



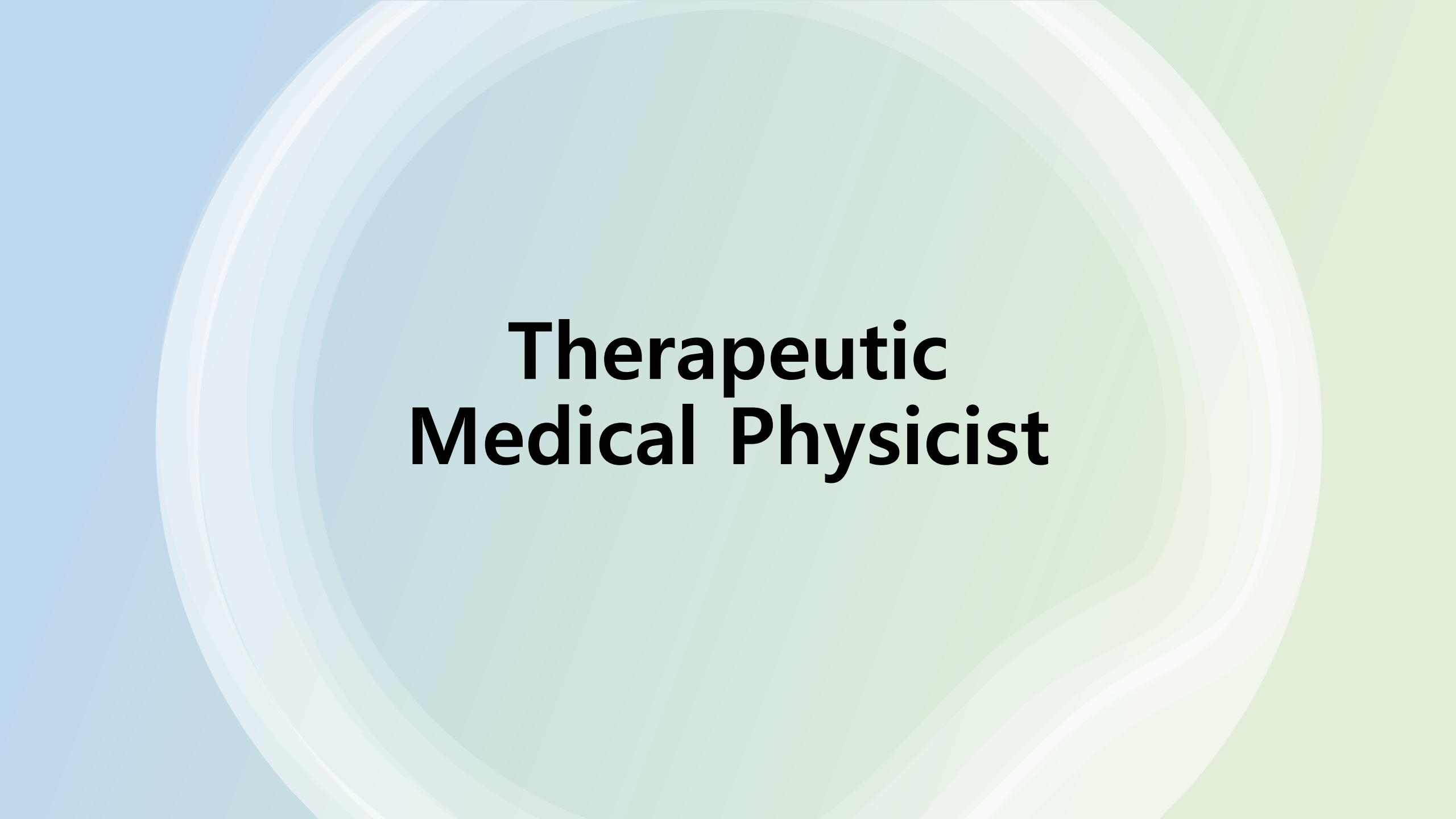
Brain perfusion

neurotransmission



Medical Health Physics

Radiation Protection
Radiation Safety Officer



Therapeutic Medical Physicist

Radiation Therapy Process

- Diagnosis, staging, consultation
- Simulation
 - *Decide patient position*
 - *Take images*
- Planning
 - *Design the treatment*
- Treatment Delivery
 - *Implement your plan*
- Response Assessment

Safe and Efficient Treatment Delivery

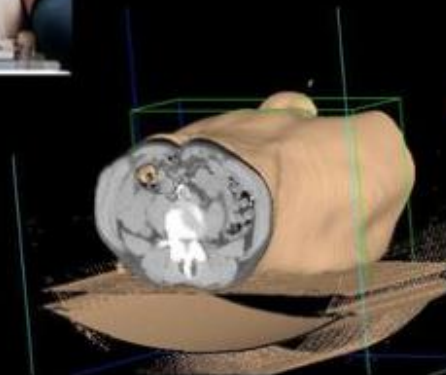
Simulation



Planning



Treatment



- Process
 - Immobilization
 - for patient positioning and reproducibility
 - Localization
 - establish a fixed coordinate system in relation to a reference point (Isocenter)
 - Modeling
 - 2D or 3D model of patient constructed through imaging
- Physicist:
 - CT scanner quality assurance
 - HU vs electron density table
 - Immobilization device assessment

Safe and Efficient Treatment Delivery

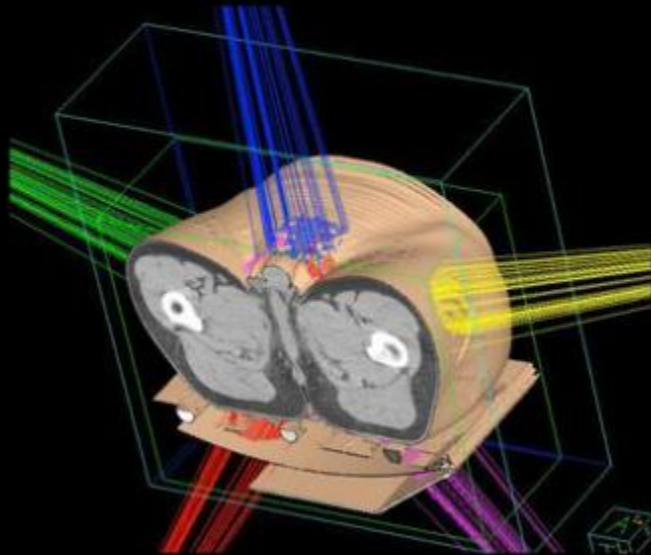
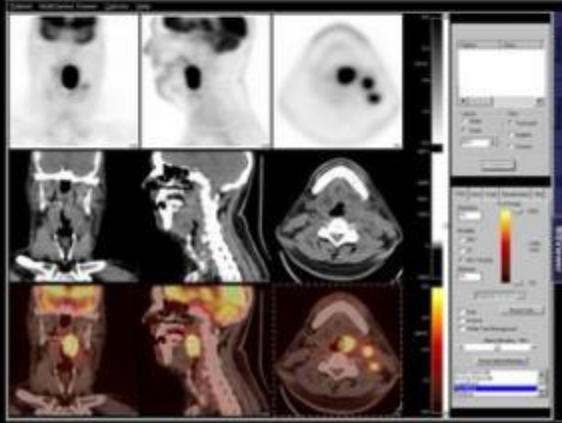
Simulation



Planning



Treatment



- Process

- Define target / critical structures
- Prescribe dose / dose limits
- Establish field portals
- Calculate dose

- Physicist:

- Machine modeling
- Dose algorithm
- Image registration
- Feasibility of treatment

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Simulation



Planning



Treatment

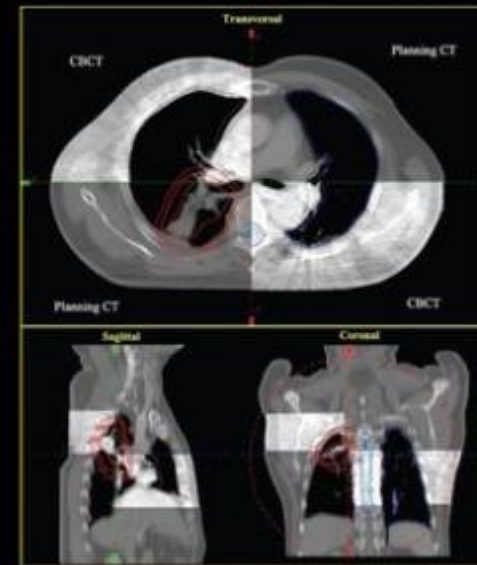
- Process

- Setup patient
- Localization
 - External beam: Set the reference point in patient to the linac isocenter
- Delivery
 - Safety checks (right patient, site, plan etc.)
 - Equipment functionality (interlocks)
 - Clearance

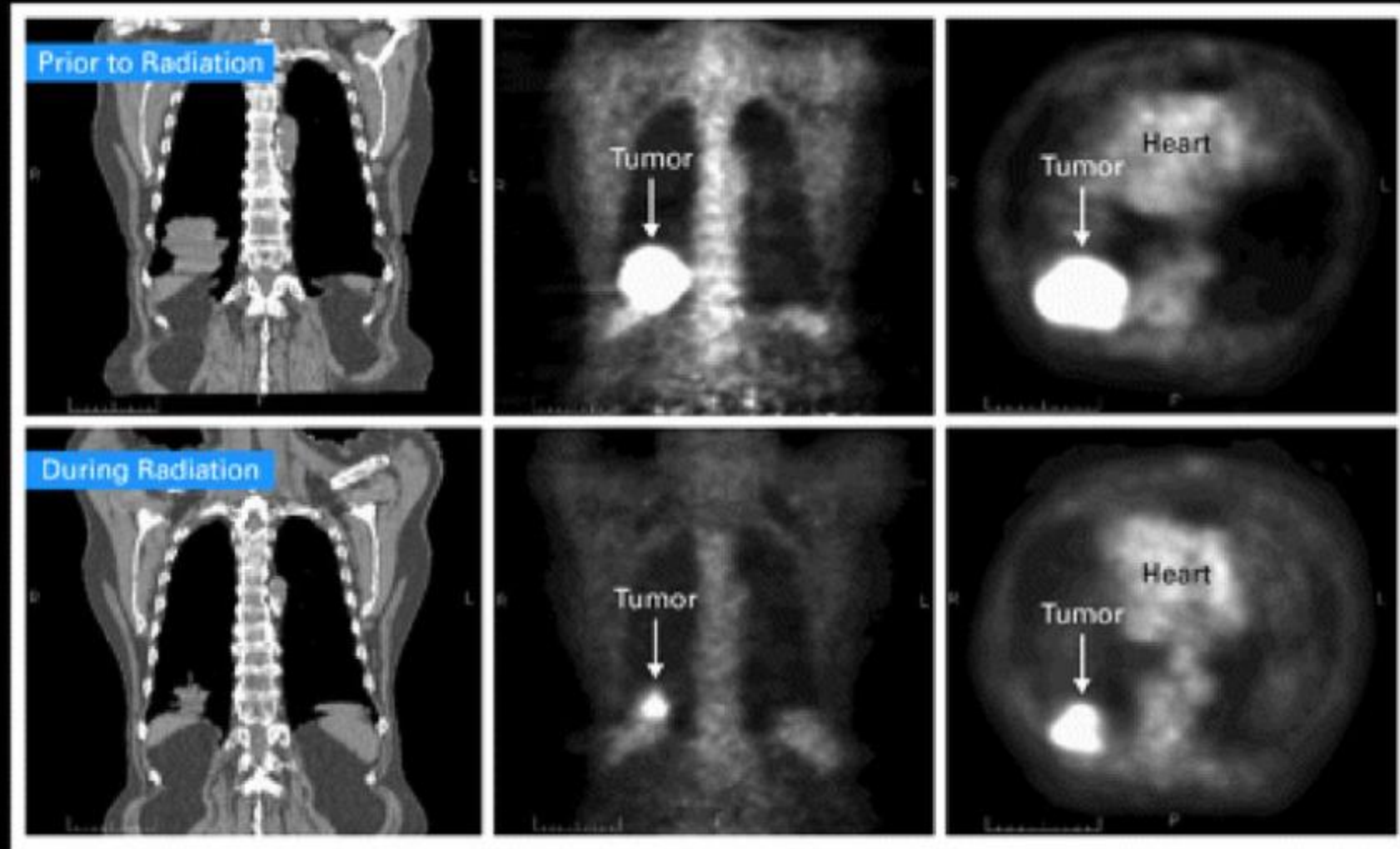


- Physicist:

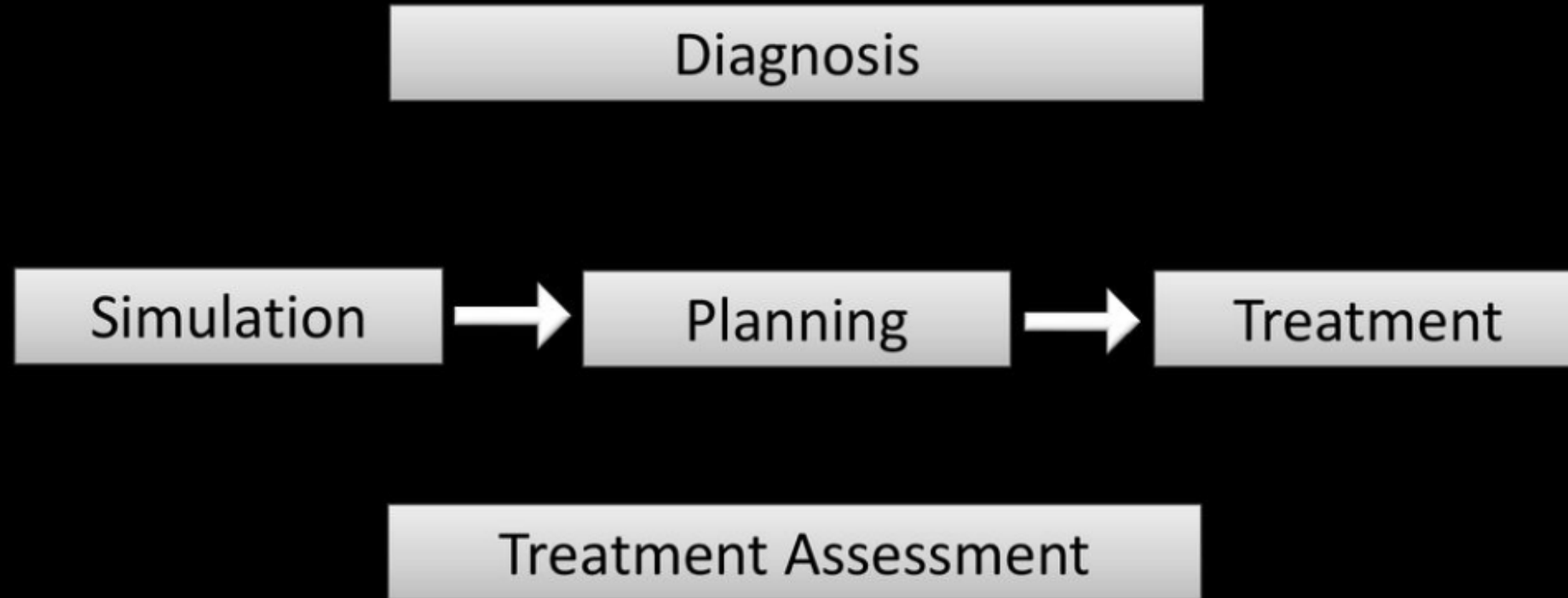
- Machine quality assurance and calibration
- Fidelity of treatment process
- Implementation of new technologies
- Workflow efficiency



Treatment Assessment



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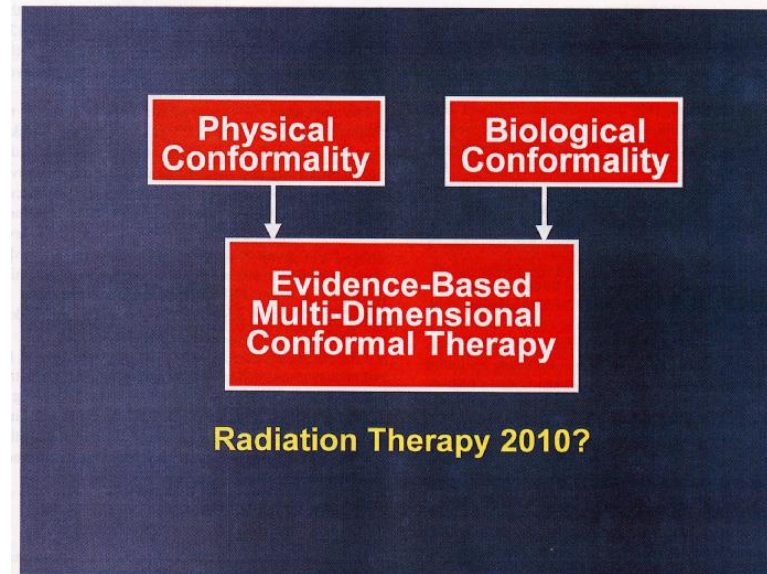
What possible issues do you see?

anatomical changes visibility of disease radiosensitivity/radioresistance patient comfort
setup uncertainty validity of assumptions during dose calcs reliable response assessment
treatment speed image registration errors normal tissue toxicity multimodality treatments

Research Area

- Imaging: X-ray, CT, MRI, PET, US, ..., new imaging modality
- Image reconstruction algorithm, noise reduction, deformable image reconstruction, image processing,
- MR sequence
- RT technology1: photon, electron, proton, helium, carbon, ..., Brachytherapy
- Scattering, pensile beam scanning, ...
- RT technology2: IMRT, VMAT, Gating, IGRT, ART
- RTP: optimization, dose calculation
- Immobilization technology,
- Quality Assurance: Dosimetry technology, application, QA protocol
- Patient Safety: collision detection/avoidance, surface imaging
- Clinical research: clinical outcome,

Physics meets biology : from physical to biological conformality



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